

課程名稱: 醫學工程概論

(Introduction to biomedical engineering)

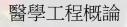


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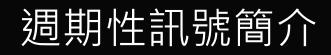


- 生物系統簡介
- 週期性訊號簡介
- 線性訊號及非線性訊號簡介
- 生醫訊號分析
- 生醫訊號臨床應用簡介











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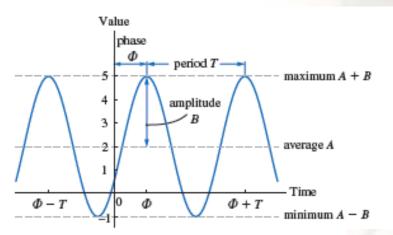
#### Sine and Cosine: A Review

In applied mathematics, angles are measured in <u>radians</u>, defined as the distance along the perimeter of the circle of radius 1.

The **basic identity** between radians and degrees is given by  $2\pi$  rad = 360°

### **Describing Oscillations with the Cosine**

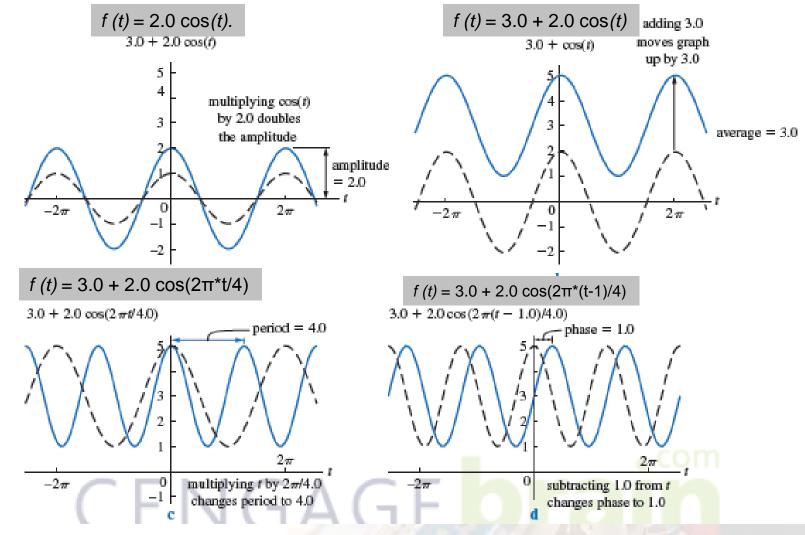
Oscillations that are shaped like the graph of the sine or cosine function are called **sinusoidal**. There are four numbers needed to describe an oscillation with the cosine function: the **average**, the <u>amplitude</u>, the <u>period</u>, and the <u>phase</u>.

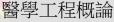


- The amplitude is the difference between the maximum and the average.
- The period is the time between successive peaks.
- The **phase** is the time of the first peak.

### Building an Oscillation by Shifting and Scaling the Cosine Function









Women have two cycles affecting body temperature: a daily and a monthly rhythm. The key facts about these two cycles are given in the following table:

	Minimum	Maximum	Average	Time of Maximum	Period
Daily cycle	36.5	37.1	36.8	2:00 p.m.	24 hours
Monthly cycle	36.6	37.0	36.8	Day 16	28 days
	37.2 37.0 36.8 36.6 36.4 36.4 36.4 0 6 12 18	perature cycle	Monthly temperature cycle 37.2 37.2 37.2 36.8 36.4 36.4 36.2 0 7 14 21 0 7 14 21 0 Time (days)		

The amplitude of a cycle is : amplitude = maximum - average. For the daily cycle, the amplitude is

daily cycle amplitude = 37.1 - 36.8 = 0.3. For the monthly cycle, the amplitude is monthly cycle amplitude = 37.0 - 36.8 = 0.2.

$$P_d(t) = 36.8 + 0.3 \cos\left(\frac{2\pi}{24}(t-14)\right)$$
.  $P_m(t) = 36.8 + 0.2 \cos\left(\frac{2\pi}{28}(t-16)\right)$ .





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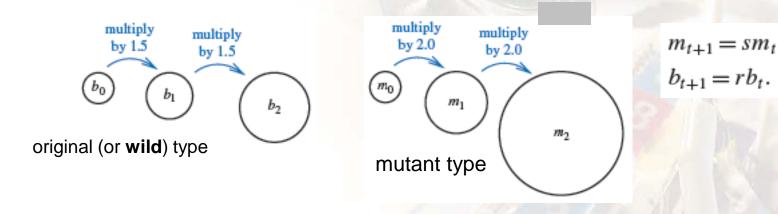
We now derive a model of two competing bacterial populations that leads naturally to a discrete-time dynamical system that is not linear. Nonlinear dynamical systems may have <u>more than one equilibrium</u>. By comparing the two equilibria, we will catch a glimpse of an important theme, <u>the stability of equilibria</u>.

Model of Selection: An invasion by mutant bacteria

If the original (or **wild**) type has a <u>per capita reproduction of 1.5</u> and the mutant type has <u>a per</u> <u>capita reproduction of 2.0</u>, the two populations will follow the discrete-time dynamical systems  $b_{t+1} = 1.5b_t$  discrete-time dynamical system for wild type

 $m_{t+1} = 2.0m_t$  discrete-time dynamical system for mutants.

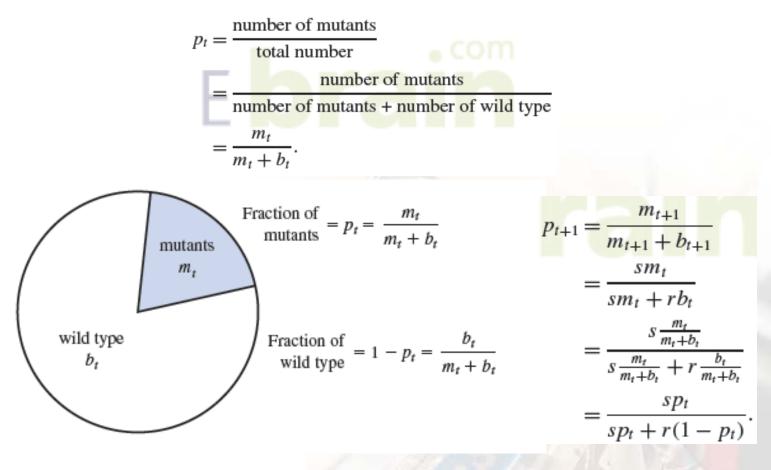
Selection occurs when the frequency of a gene (the mutation) changes over time.







A new variable called *pt* was defined to be the fraction of mutants at time *t*. Then



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**Example** Finding the Updated Fraction

If  $m_t = 2.0 \times 10^5$  and  $b_t = 3.0 \times 10^6$  (Example 1.10.1), the updated populations are

$$m_{t+1} = 2.0m_t = 4.0 \times 10^5$$
  
 $b_{t+1} = 1.5b_t = 4.5 \times 10^6.$ 

The updated fraction of the mutant type,  $p_{t+1}$ , is

$$p_{t+1} = \frac{4.0 \times 10^5}{4.0 \times 10^5 + 4.5 \times 10^6} = 0.0816.$$

We can follow these same steps to find the discrete-time dynamical system for  $p_t$ . By definition

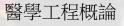
$$p_{t+1} = \frac{m_{t+1}}{m_{t+1} + b_{t+1}}$$

Using the discrete-time dynamical systems for the two types (Equation 1.10.1), we find

$$p_{t+1} = \frac{2.0m_t}{2.0m_t + 1.5b_t}$$

$$p_{t+1} = \frac{2.0 \frac{m_t}{m_t + b_t}}{2.0 \frac{m_t}{m_t + b_t} + 1.5 \frac{b_t}{m_t + b_t}}.$$

$$p_{t+1} = \frac{2.0 p_t}{2.0 p_t + 1.5(1 - p_t)}.$$

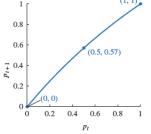


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If  $p_t = 0.0625$ , the discrete-time dynamical system tells us that

$$p_{t+1} = \frac{2.0 \cdot 0.0625}{2.0 \cdot 0.0625 + 1.5(1 - 0.0625)} = 0.0816.$$



The discrete-time dynamical system for the fraction is not linear because it involves division. The graph of the function is curved. We plotted it by substituting in representative values for a fraction, which must lie between 0 and 1.

The equilibria of this discrete-time dynamical system are found by solving

 $p^* = \frac{2.0p^*}{2.0p^* + 1.5(1-p^*)}$ the equation for the equilibrium  $p^{*}(2.0p^{*} + 1.5(1 - p^{*})) = 2.0p^{*}$ multiply through by denominator  $p^{*}(2.0p^{*}+1.5(1-p^{*})) - 2.0p^{*} = 0$ move everything to one side  $p^{*}(2.0p^{*} + 1.5(1 - p^{*}) - 2.0) = 0$ factor out  $p^*$  $p^{*}(2.0p^{*}+1.5-1.5p^{*}-2.0)=0$ multiply out terms in parentheses  $p^*(0.5p^* - 0.5) = 0$ simplify

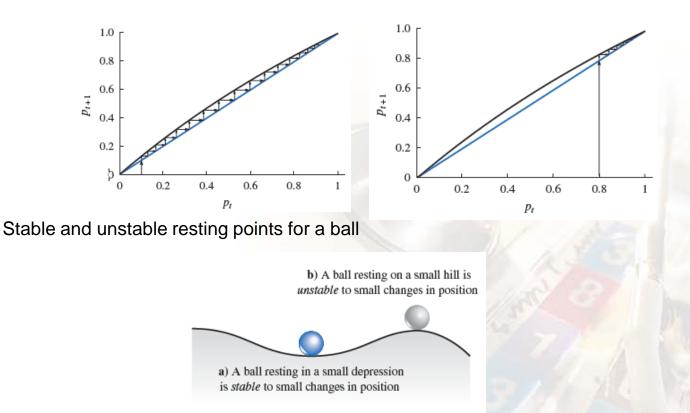
Extinction of the mutant (at p = 0), extinction of the wild type (at p = 1)

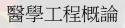


### **Stable and Unstable Equilibria**



If we started **exactly** at  $p_0 = 0$ , the solution would remain at pt = 0 for all times *t*. Similarly, if we started **exactly** at  $p_t = 1$ , the solution would remain at pt = 1 for all times *t*. The two equilibria behave quite differently, however, if our starting point is nearby. A solution starting **near**  $p_0 = 0$  moves steadily **away** from the equilibrium. A solution starting **near**  $p_0 = 1$  moves **toward** the equilibrium.



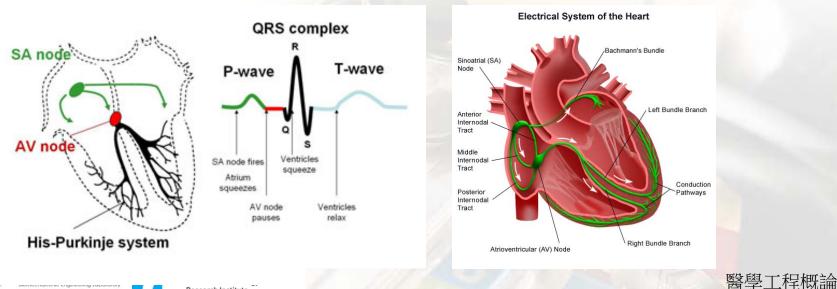






### **An Excitable Systems: The Heart**

- The sinoatrial node (SA node) is the pacemaker, sending regular signals to the • atrioventrical node (AV node). The AV node then tells the heart to beat if conditions are suitable.
- Our goal is to understand how simple changes in the parameters of a heart can produce heartbeat patterns called **second-degree block**. With these syndromes, people's hearts either beat half as often as they should or beat normally for a while, skip a beat, and return to beating.









#### **Membrane Potential**

Membrane potentials in cells are determined primarily by three factors:

- 1) the concentration of ions on the inside and outside of the cell;
- 2) the permeability of the cell membrane to those ions through specific ion channels;
- 3) by the activity of electrogenic pumps (e.g. Na<sup>±</sup> /K<sup>±</sup> –ATPase and Ca<sup>±±</sup> transport pumps) that maintain the ion concentrations across the membrane.

#### Equilibrium potential for K<sup>+</sup> (E<sub>K</sub>; Nernst potential)

$$E_{K} = \frac{-61}{z} \log \frac{[K^{+}]_{i}}{[K^{+}]_{o}} = -96 \text{ mV}$$

(where  $[K^+]_i = 150 \text{ mM}$  and  $[K^+]_o = 4 \text{ mM}$ ; and z=1 because K<sup>+</sup> is monovalent)

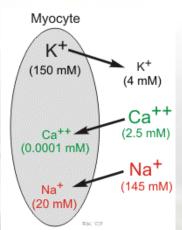
Equilibrium potential for Na<sup>+</sup>(E<sub>Na</sub>)

$$E_{Na} = \frac{-61}{z} \log \frac{[Na^+]_i}{[Na^+]_o} = +52 \text{ mV}$$

(where  $[Na^+]_i = 20 \text{ mM}$  and  $[Na^+]_o = 145 \text{ mM}$ ; and z=1 because Na<sup>+</sup> is monvalent)

Equilibrium potential for Ca<sup>++</sup> (E<sub>Ca</sub>)

$$E_{Ca} = \frac{-61}{z} \log \frac{[Ca^{++}]_i}{[Ca^{++}]_o} = +134 \text{ mV}$$



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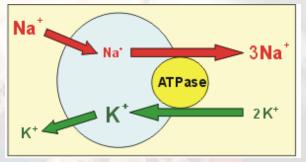




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#### **Membrane Potential**

- To maintain the concentration gradients for Na<sup>+</sup> and K<sup>+</sup>, it is necessary to transport Na<sup>+</sup> out of the cell and K<sup>+</sup> back into the cell. There is located on the sarcolemma an energy dependent (ATP-dependent) pump system Na<sup>+</sup>/K<sup>+</sup>-ATPase) that that performs this function.
- Pump is electrogenic in nature because it extrudes 3 Na<sup>+</sup> for every 2 K<sup>+</sup> entering the cell.
- Inhibition of this pump, therefore, causes depolarization resulting not only from changes in Na<sup>+</sup> and K<sup>+</sup> concentration gradients, but also from the loss of an electrogenic component of the membrane potential.
- By pumping more positive changes out of the cell than into the cell, the pump activity creates a negative potential within the cell.
- Small increases in external K<sup>+</sup> can stimulate the pump activity and thereby cause hyperpolarization.





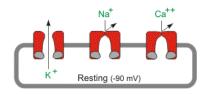


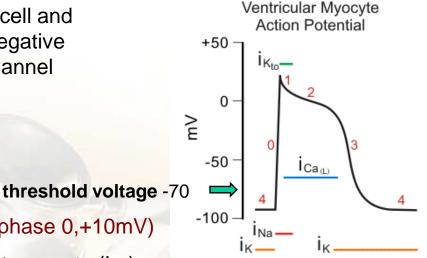
#### **Action Potentials**

Many cells in the body have the ability to undergo a transient repolarization and depolarization that is either triggered by external mechanisms.

Resting membrane potential (phase 4, about -90 mV)

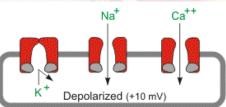
Positive potassium ions are leaving the cell and making the membrane potential more negative inside. At the same time, fast sodium channel and slow calcium channels are closed.





When depolarized to a **threshold voltage** (phase 0,+10mV)

Caused by a transient increase in fast Na<sup>+</sup> currents (I<sub>Na</sub>), due to the opening of sodium channels, and concomitant outward directed K<sup>+</sup> currents as the potassium channel closed.



http://www.cvphysiology.com/Arrhythmias/A010.htm





#### **Action Potentials**

#### Repolarization (phase 1)

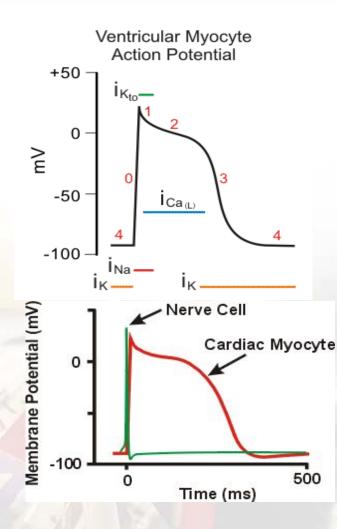
represents an initial repolarization that is caused by the opening of a special type of transient outward K<sup>+</sup> channel (K<sub>to</sub>), which causes a short-lived, hyperpolarizing outward K<sup>+</sup> current ( $I_{Kto}$ ).

#### Repolarization (phase 2)

Large increase in slow inward gCa<sup>++</sup> occurring at the same time and the transient nature of  $I_{Kto}$ , the repolarization is delayed and there is a plateau phase in the action potential.

#### Repolarization (phase 3)

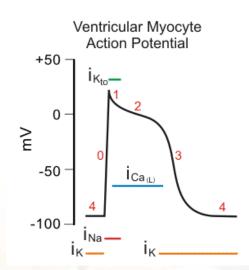
Occurs when  $gK^+$  (and therefore  $I_K$ ) increases, along with the inactivation of Ca<sup>++</sup> channels (decreased  $gCa^{++}$ ).

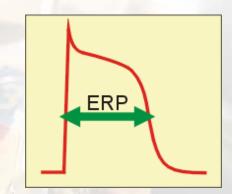




#### **Effective Refractory Period**

- Once an action potential is initiated, there is a period of time comprising <u>phases 0, 1, 2, and</u> <u>part of phase 3</u> that a new action potential cannot be initiated. This is termed the effective refractory period (ERP) or the absolute refractory period (ARP) of the cell.
- During the ERP, stimulation of the cell by an adjacent cell undergoing depolarization does not produce new, propagated action potentials. The ERP acts as a <u>protective mechanism</u> in the heart by preventing multiple, compounded action potentials from occurring (i.e., it limits the frequency of depolarization and therefore heart rate).





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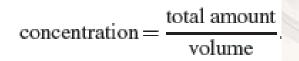


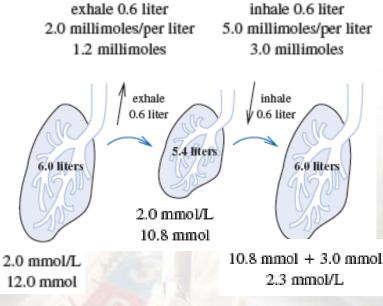


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#### A Model of Gas Exchange in the Lung

- An adult male lung has a volume of about <u>6.0 L</u> when full. With each breath, <u>0.6 L</u> of the air in the lungs are exhaled, and replaced by 0.6 L of outside (or **ambient**) air.
- Suppose further that the lung contains a particular chemical with a concentration of <u>2.0</u> <u>mmol/L</u> before exhaling that the lungs contain.
- The ambient air has a chemical concentration of <u>5.0 mmol/L</u>. What is the chemical concentration after one breath?





total amount = concentration X volume.

( A millimole is 6.02x 10<sup>20</sup> molecules)

Assumption: Neither air nor chemical is produced or used while breathing.



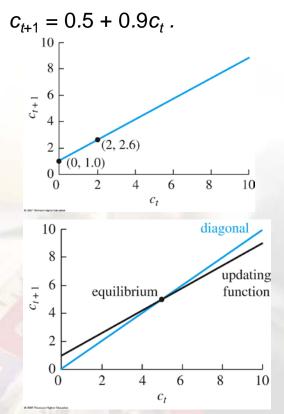


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Breathing creates a discrete-time dynamical system. The original concentration of 2.0 mmol/L is updated to 2.3 mmol/L after a breath.

Step	Volum (L)	Total e Chemical ( (mmol)	Concentration (mmol/L)	What We Did
Air in lungs before breath	6.0	$6.0c_t$	$c_t$	Multiplied volume of lungs (6.0) by concentration ( $c_t$ ) to get 6.0 $c_t$ .
Air exhaled	0.6	0.6ct	$c_t$	Multiplied volume exhaled (0.6) by concentration ( $c_t$ ) to get $0.6c_t$ .
Air in lungs after exhalation	5.4	$5.4c_t$	$c_t$	Multiplied volume remaining (5.4) by concentration $(c_t)$ to get 5.4 $c_t$ .
Air inhaled	0.6	3.0	5.0	Multiplied volume inhaled (0.6) by ambient concentration (5.0) to get 7.5.
Air in lungs after breath	6.0	3.0 + 5.4c <sub>t</sub>	$0.5 + 0.9c_t$	Added inhaled chemical (3.0) to remaining chemical ( $+5.4c_f$ ) and divided by volume (6.0) to get $0.5 + 0.9c_t$ .

Discrete-time dynamical system



The solutions of the updating equation are equilibria.

$c^* = 0.5 + 0.9c^*$	the original equation
$c^* - 0.9c^* = 0.5$	subtract $0.9c^*$ to get unknowns on one side
$0.1c^* = 0.5$	do the subtraction
$c^* = \frac{0.5}{0.1} = 5.0.$	divide by 0.1

The equilibrium value is 5.0 mmol/L.

 $C_{t+1} = 0.5 + 0.9 \text{ x} 5.0 = 5.0 = C_t$ 



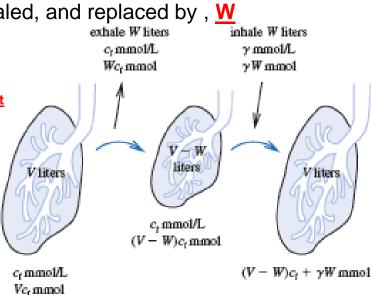
#### A "General" Model of Gas Exchange in the Lung

- An adult male lung has a volume of about <u>V</u> liter when full. With each breath, <u>W</u> liter of the air in the lungs are exhaled, and replaced by , <u>W</u> liter of outside (or **ambient**) air.
- Suppose further that the lung contains a particular chemical with a concentration of <u>c</u><u>mmol/L</u> before exhaling that the lungs contain.
- The ambient concentration of chemical is γ mmol/L ("gamma").

Discrete-time dynamical system

$$c_{t+1} = \frac{c_t(V - W) + \gamma W}{V}$$
$$= \frac{c_t V - c_t W + \gamma W}{V}$$
$$= c_t - c_t \frac{W}{V} + \gamma \frac{W}{V}.$$

 $q = \frac{W}{V} =$  fraction of air exchanged



General lung discrete-time dynamical system

 $c_{t+1} = (1-q)c_t + q\gamma.$ 

The term  $c_{t+1}$  is a **weighted average** of the old concentration  $c_t$  and the ambient concentration  $\gamma$ .

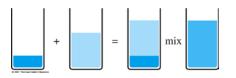
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**Definition** A weighted average of two values x and y is a sum of the form qx + (1 - q) y for some value of q between 0 and 1.



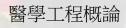
Suppose 1.0 L of liquid with a concentration of 10.0 mmol/L of salt are mixed with 3.0 L of liquid with a concentration of 5.0 mmol/L of salt. What is the concentration of the resulting mixture?

 $0.25 \times 10.0 \text{ mmol/L} + 0.75 \times 5.0 \text{ mmol/L} = 6.25 \text{ mmol/L}.$ 

Suppose 1.0 L of liquid with a concentration of 10.0 mmol/L of salt are mixed with 3.0 L of liquid with a concentration of 5.0 mmol/L of salt and 1.0 L of liquid with a concentration of 2.0 mmol/L of salt. What is the concentration of the resulting mixture?

0.20 x 10.0 mmol/L + 0.60 x 5.0 mmol/L + 0.20 x 2.0 mmol/L = 5.4 mmol/L.







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#### A "Absorption" Model of Gas Exchange in the Lung

- An adult male lung has a volume of about <u>V</u> liter when full. With each breath, <u>W</u> liter of the air in the lungs are exhaled, and replaced by , <u>W</u> liter of outside (or **ambient**) air.
- Suppose further that the lung contains a particular chemical with a concentration of <u>c</u><sub>t</sub> <u>mmol/L</u> before exhaling that the lungs contain.
- The ambient concentration of chemical is γ mmol/L ("gamma").
- Suppose that a fraction *q* of air is exchanged each breath, and that a fraction *α* of chemical is absorbed

#### Lung discrete-time dynamical system

$$c_{t+1} = (1 - q)(1 - \alpha)c_t + q\gamma.$$

absorb a inhale W L fraction  $\alpha$  exhale W liters  $\gamma$  mmol/L  $V_{L}$   $V_{L}$ 





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#### Example: Absorption of Oxygen by the Lung

Consider again a lungs that has a volume of 6.0 L(V) and that replaces 0.6 L(W) each breath with ambient air (q = 0.6/6). Suppose that we are tracking oxygen, with an ambient concentration of 21% ( $\gamma$ ), and assume that 30% ( $\alpha$ ) of the oxygen in the lungs is absorbed each breath.

The discrete-time dynamical system is then

$$c_{t+1} = 0.9 \times 0.7 c_t + 0.1 \times 0.21 = 0.63 c_t + 0.021.$$

The equilibrium concentration in the lungs then becomes

$$c^* = 0.63c^* + 0.02$$
  
 $0.37c^* = 0.021$   
 $c^* = 0.057.$ 

The equilibrium concentration of oxygen in the lungs, which is equal to the concentration of oxygen in the air breathed out, would be about 5.7%, or roughly <u>one</u> <u>fourth of the ambient concentration</u>.

$$c^* = (1 - q)(1 - \alpha)c^* + q\gamma$$

$$c^* - (1 - q)(1 - \alpha)c^* = q\gamma$$

$$c^*(1 - (1 - q)(1 - \alpha)) = q\gamma$$

$$c^* = \frac{q\gamma}{1 - (1 - q)(1 - \alpha)}.$$

Total absorbed per breath =  $\alpha c * V$