



臺北醫學大學



# Biomedical Imaging

## 生物醫學影像學

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2013/03/18

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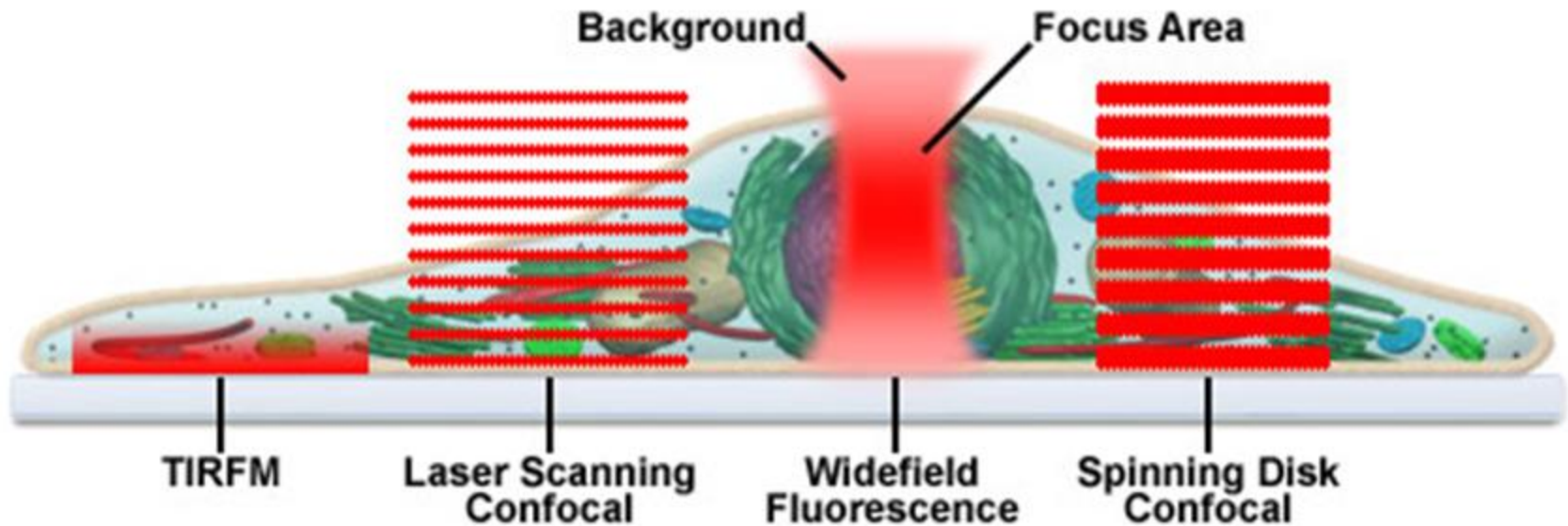
# Course Outline

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1. Course Introduction
2. Basic Optics and Light Microscopes
3. Fluorescence/Confocal/TIRF Microscopes
4. FRET Techniques and Photo-Spectroscopic Imaging
5. Single Molecule Detection
6. Cell Imaging
7. Atomic Force Microscopy (AFM)
8. Scanning Electron Microscope (SEM)
9. Transmission Electron Microscopy (TEM)
10. Digital Image Processing Using MATLAB

# Imaging Modes in Optical Microscopy

## Fluorescence Imaging Modes in Live-Cell Microscopy



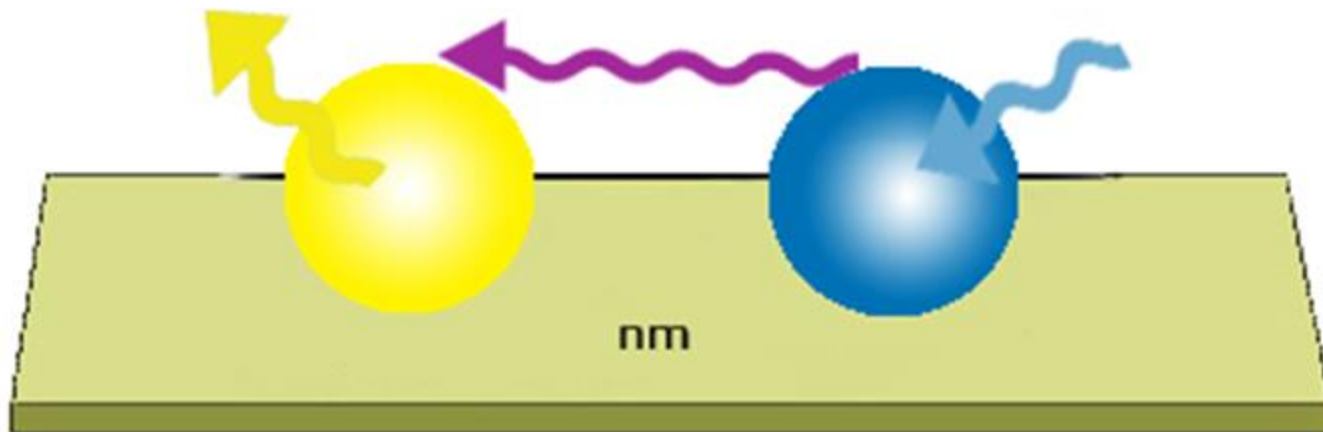
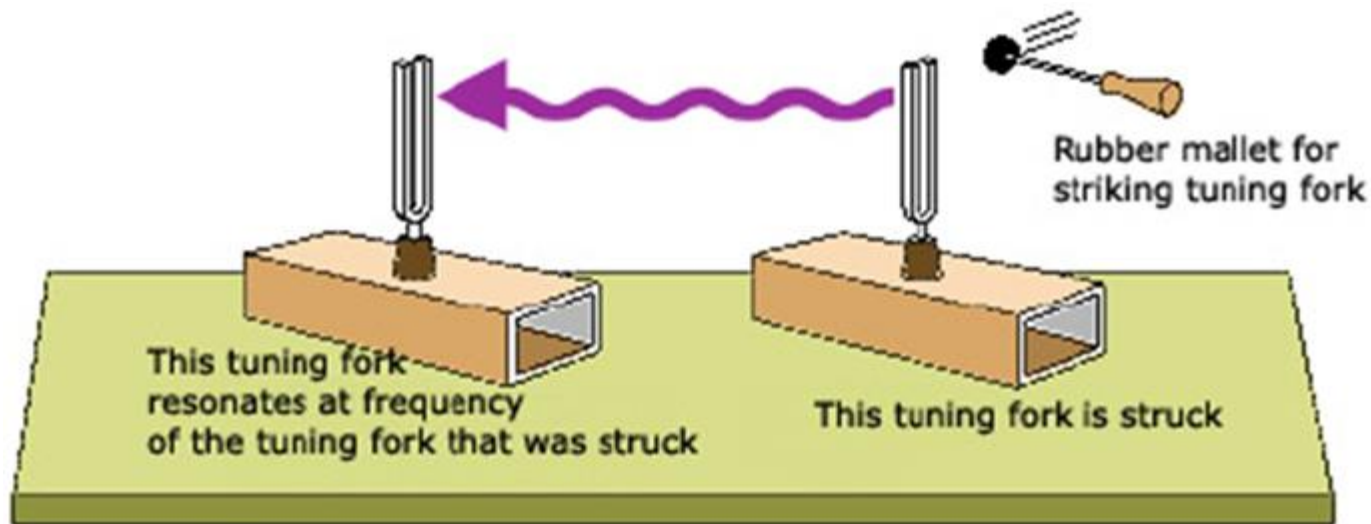
A majority of the live-cell imaging investigations are conducted with adherent mammalian cells, which are positioned within 10 micrometers of the coverslip-medium interface.



# Part I

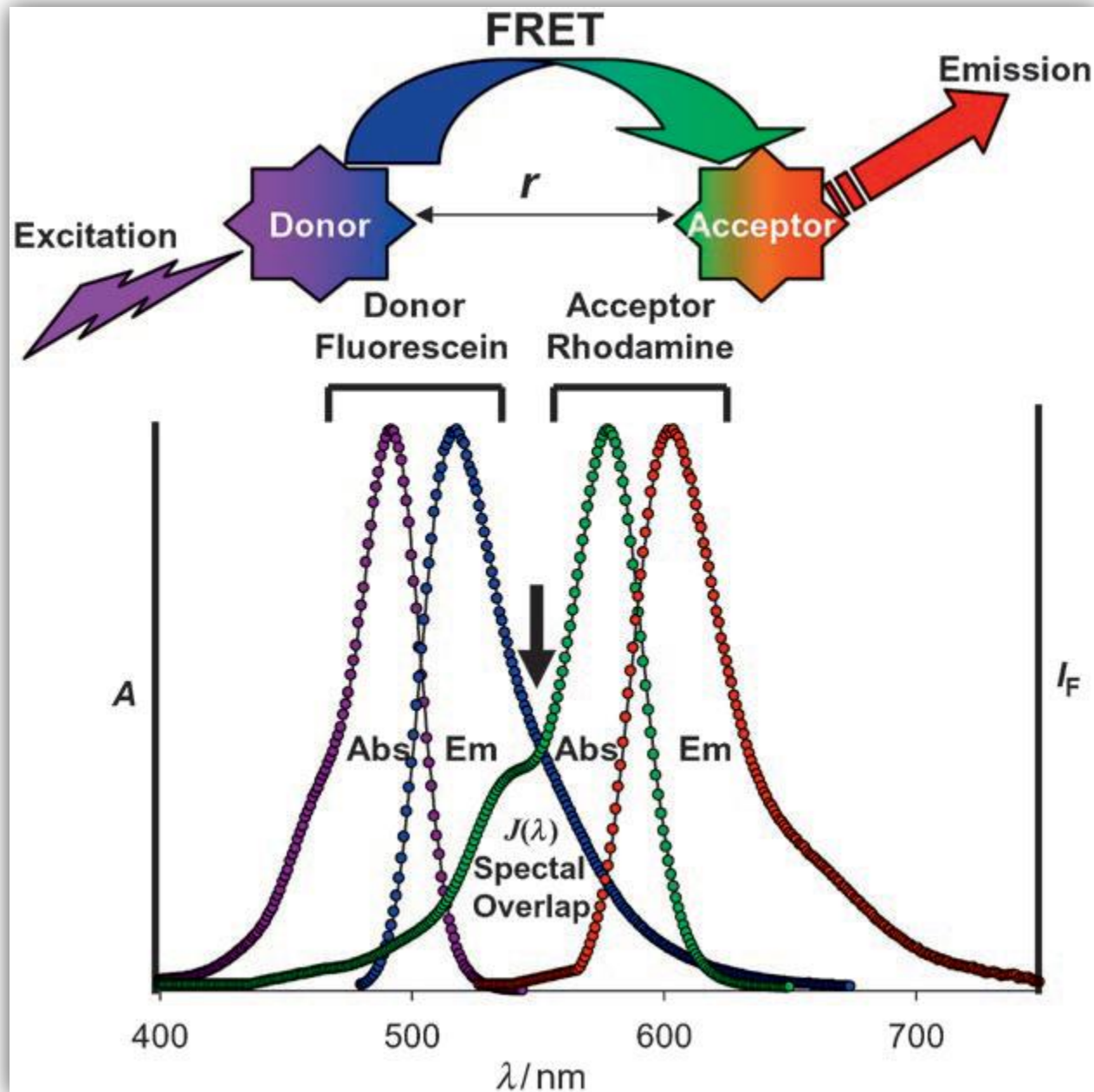
## Fluorescence Resonance Energy Transfer (FRET) Technique

# Tuning Fork Analogy for Resonance Energy Transfer



Theodore Förster in 1948

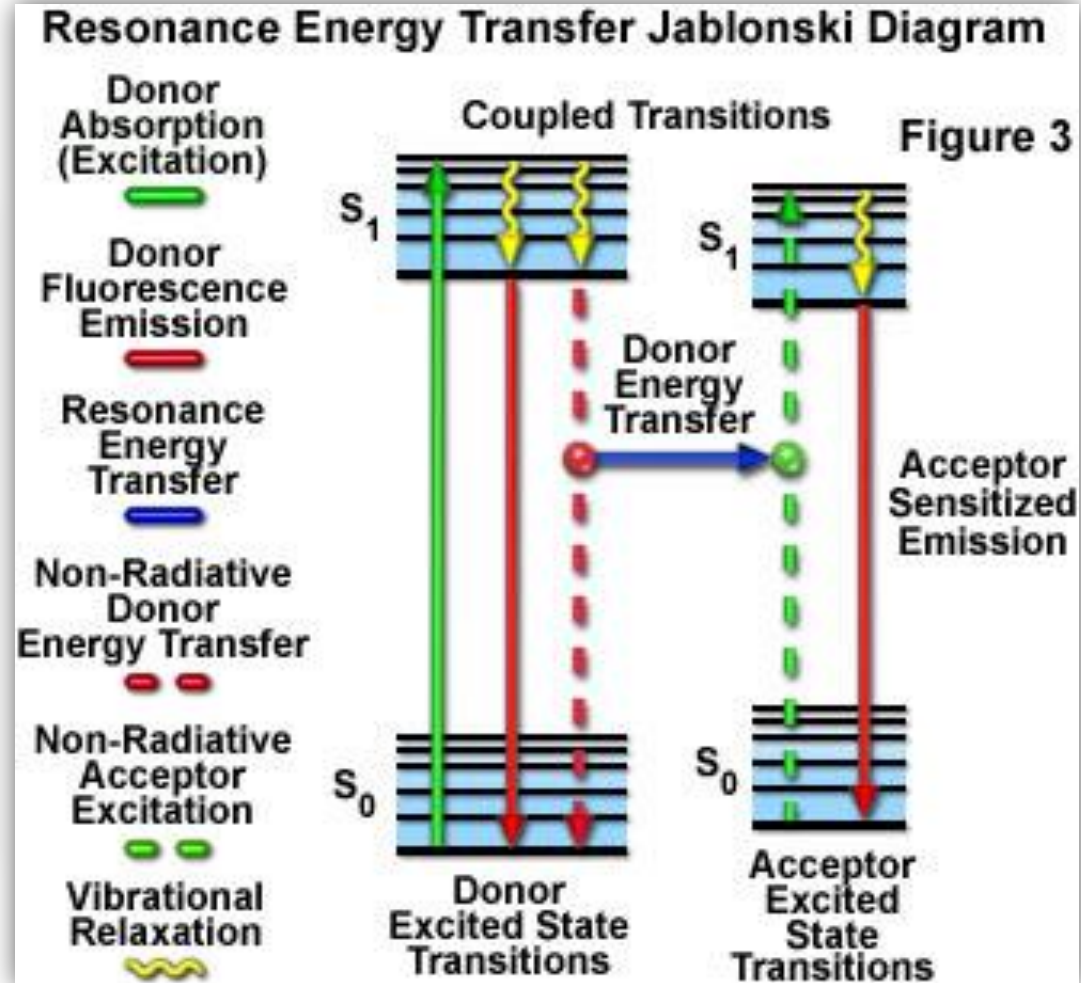
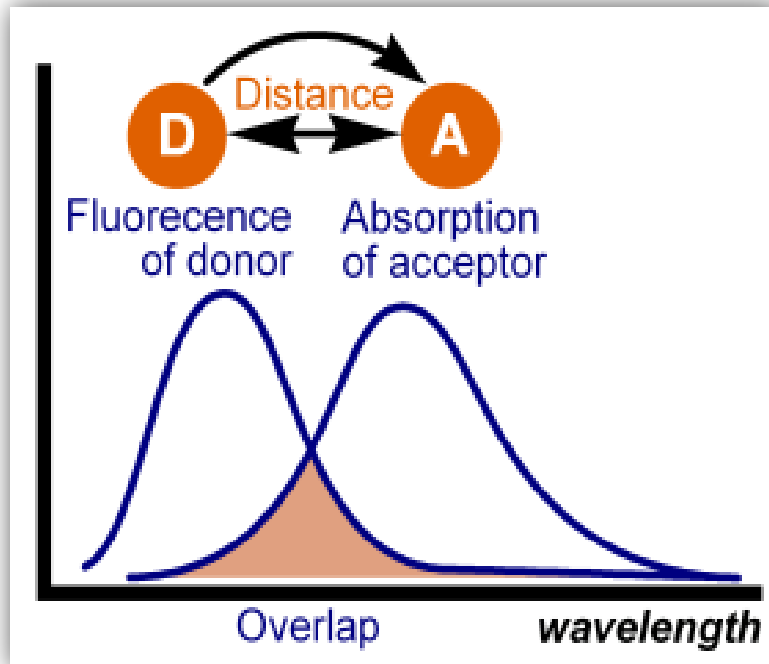
# Fluorescence Resonance Energy Transfer (FRET)





# Förster Resonance Energy Transfer (FRET)

- Based on the principles published by Theodore Förster in 1948
- FRET involves the transfer of energy between oscillating dipoles of similar resonance frequency

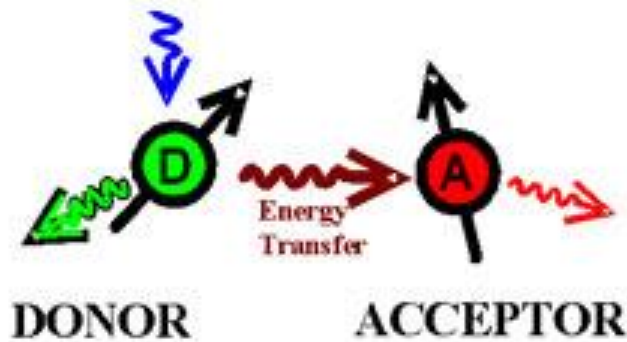


# Förster Resonance Energy Transfer (FRET)

## ➤ Energy transfer efficiency :

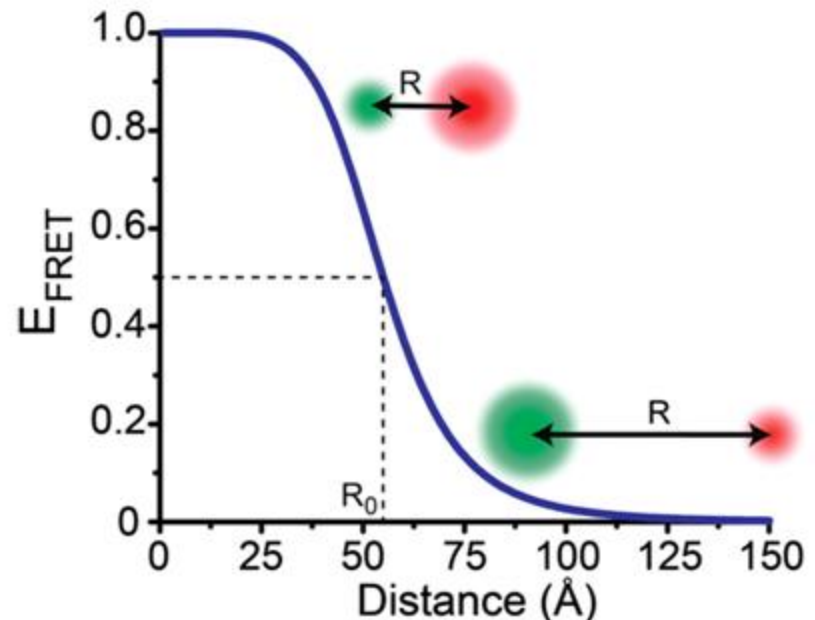
- Degree of **spectral overlap** between donor fluorescence emission and acceptor absorption
- **Inversely proportional to 6<sup>th</sup> power** of the distance between fluorophores
- **~ 10 nm**

“Spectroscopic Ruler”



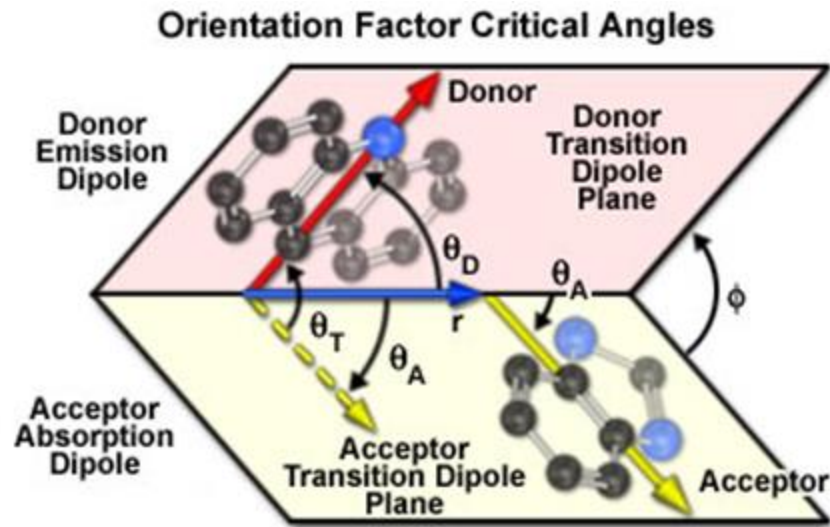
$$E = \frac{1}{1 + \left(\frac{R}{R_0}\right)^6}$$

$R_0$ =50% transfer efficiency distance  
3nm~7nm

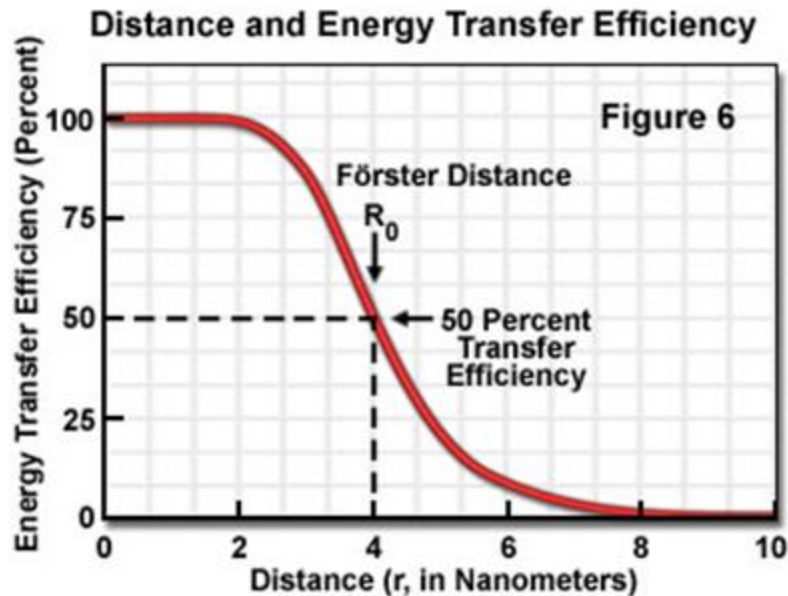
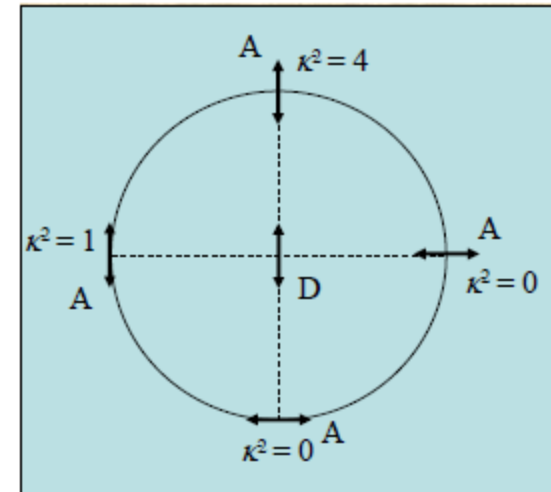




# Principles of Fluorescence Resonance Energy Transfer



**Dipole - dipole coupling**



**FRET efficiency is given by**

$$E = \frac{1}{1 + \left(\frac{R}{R_0}\right)^6}$$

# Förster Resonance Energy Transfer (FRET)

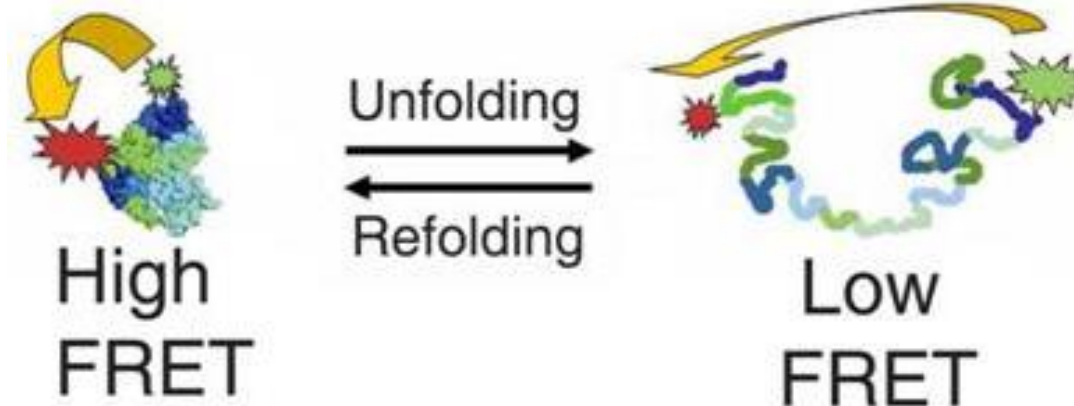
## Calculation of the distance between fluorophores

- Detection of target analytes
- Analysis of biomolecular interactions
- **Single molecule analysis**
  - Protein folding/unfolding
  - Protein dynamics
- **Living cell analysis**

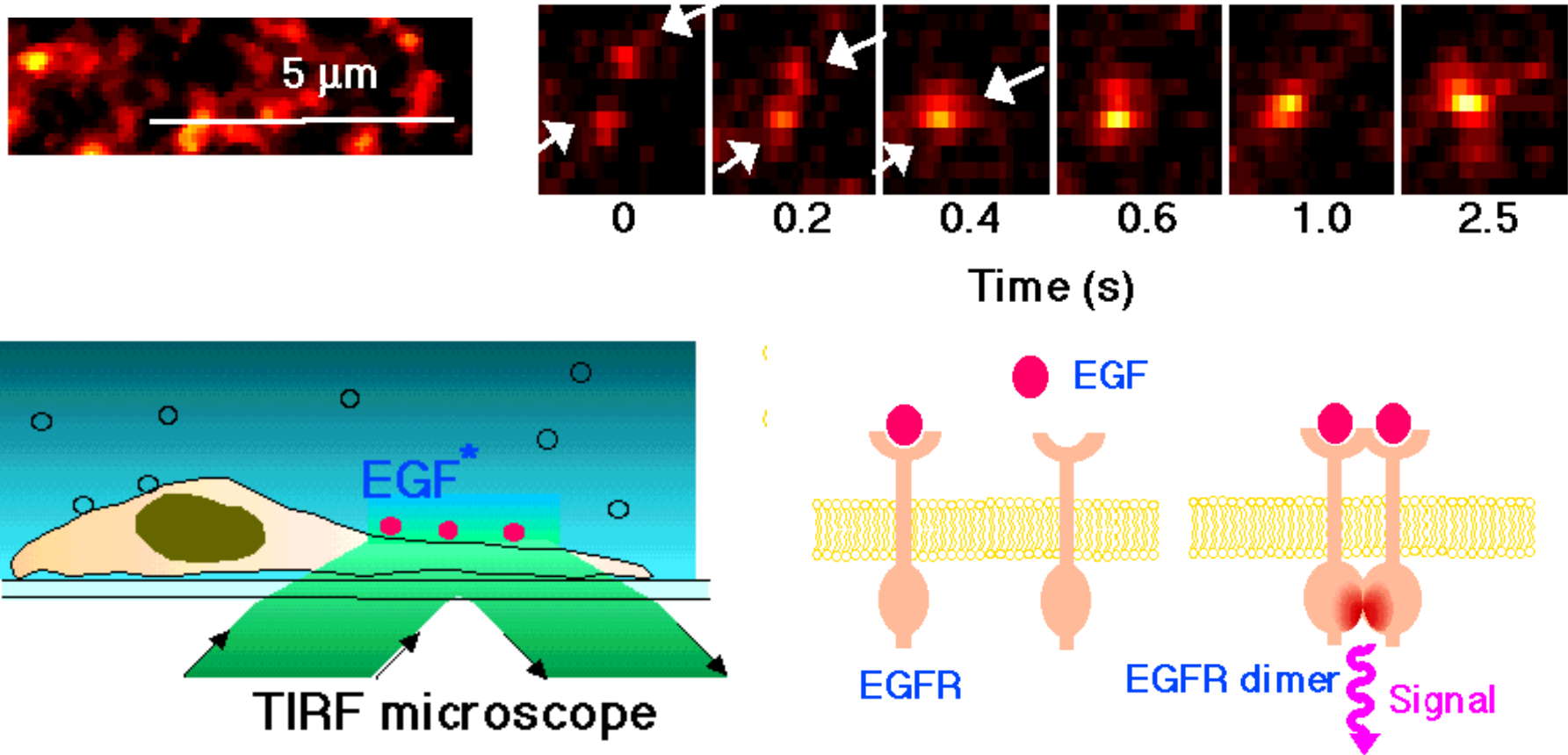
FRET efficiency is given by

$$E = \frac{1}{1 + \left(\frac{R}{R_0}\right)^6}$$

$$E_{\text{FRET}} = \frac{I_A}{(I_D + I_A)}$$



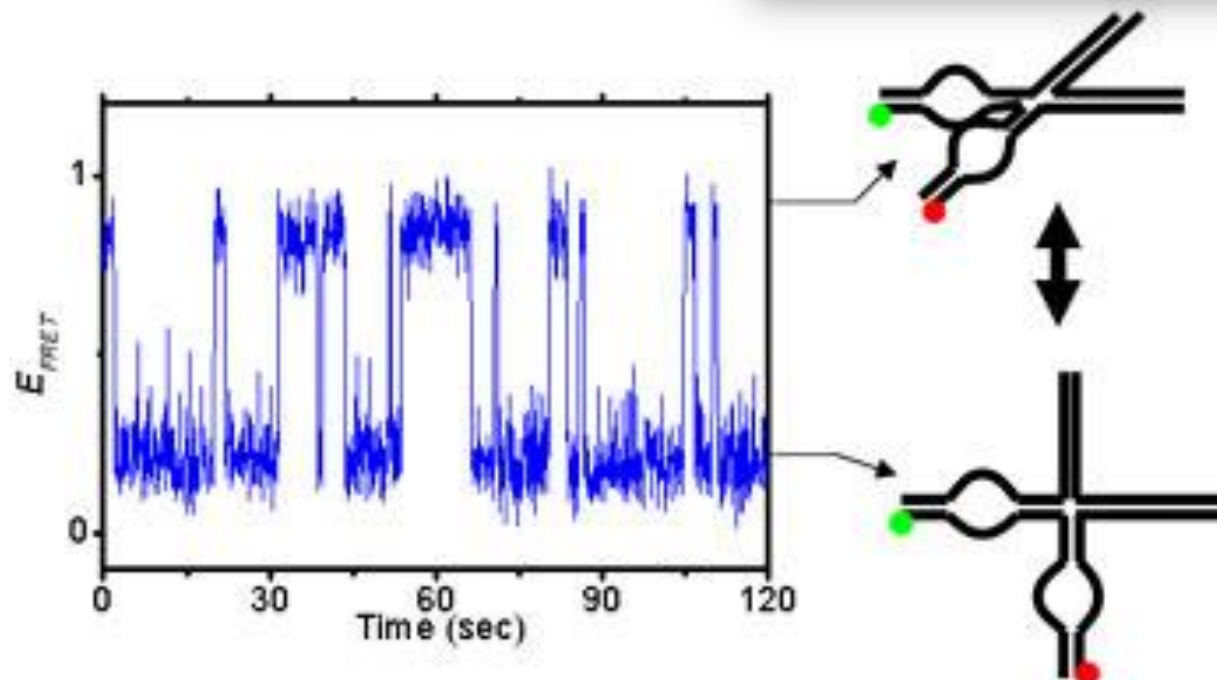
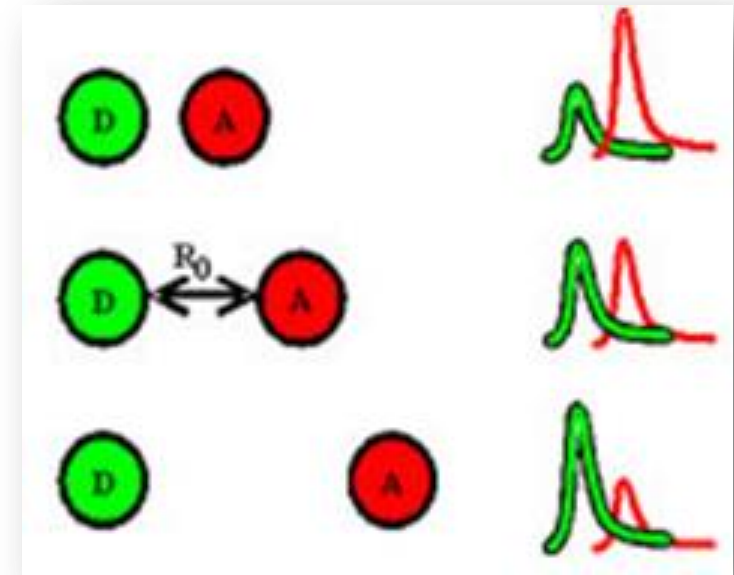
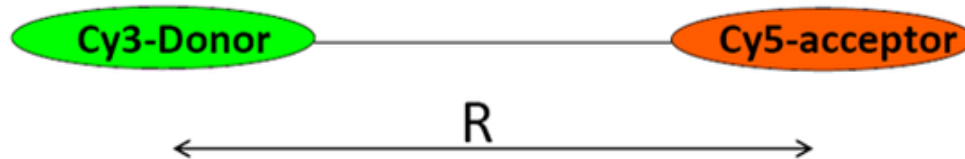
**Cell signaling.** Fluorescently labeled epidermal growth factor (EGF) was visualized on the cell surface. A single EGF molecule can be seen as a spot and a time sequence of images shows dimerization of the EGF/EGF receptor, triggering transmission of signal.



# Quantitative analysis using FRET

FRET efficiency is given by

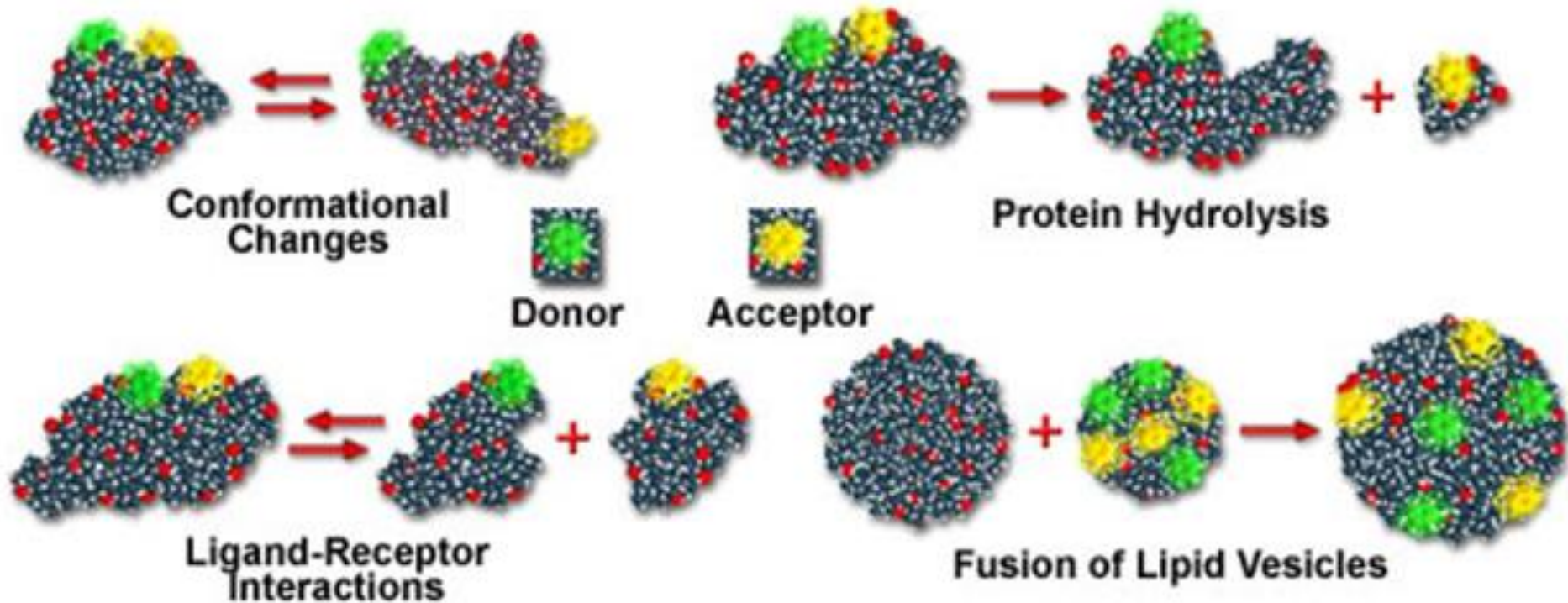
$$E = \frac{1}{1 + \left(\frac{R}{R_0}\right)^6}$$





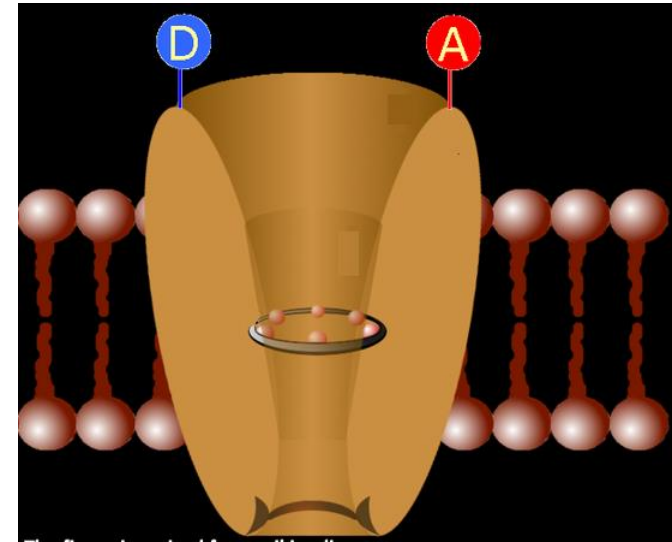
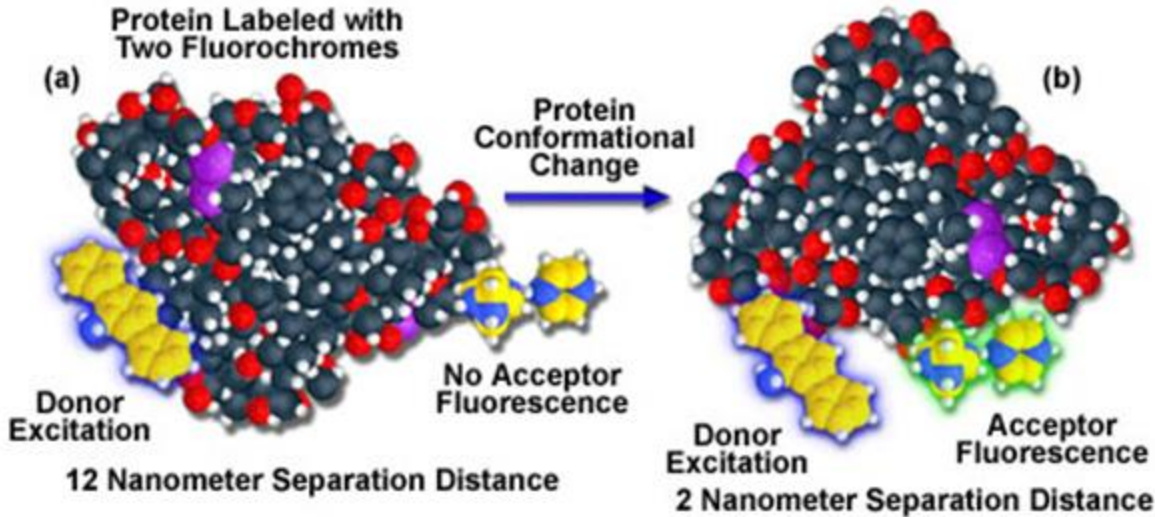
# Quantitative analysis using FRET

## Biomolecular Fluorescence Resonance Energy Transfer Applications

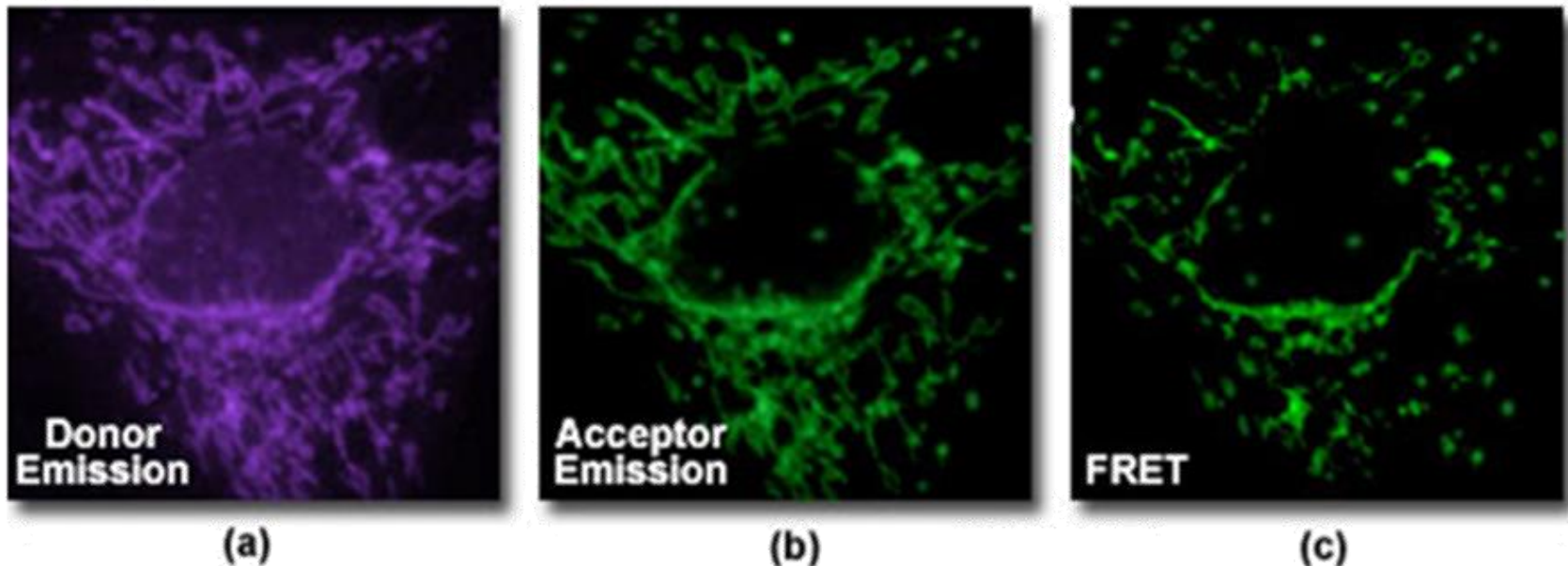


# Quantitative analysis using FRET

## Intramolecular Fluorescence Resonance Energy Transfer (FRET)



## Mitochondrial Protein-Protein Association with FRET

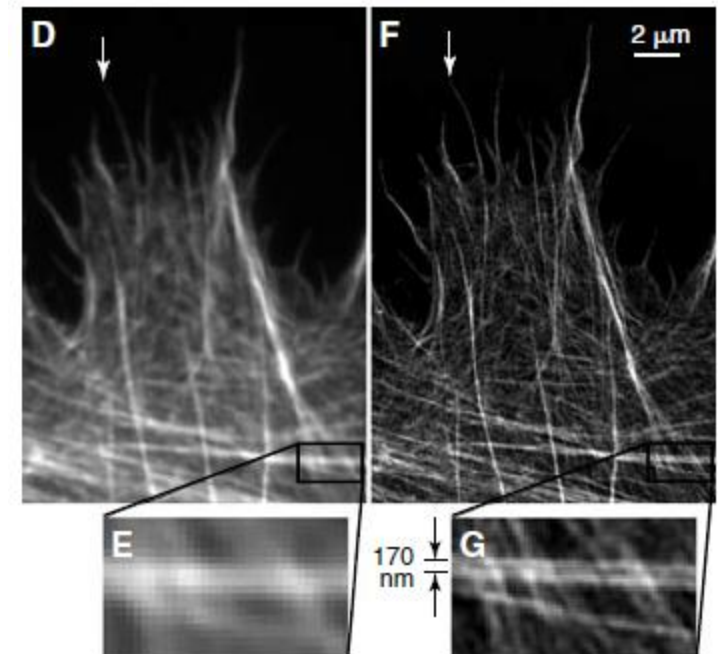
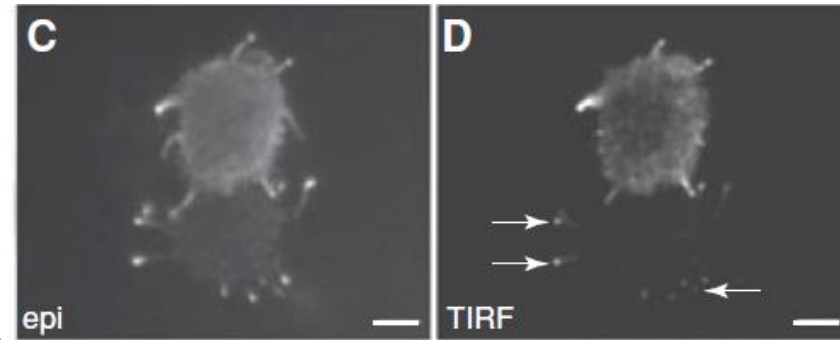
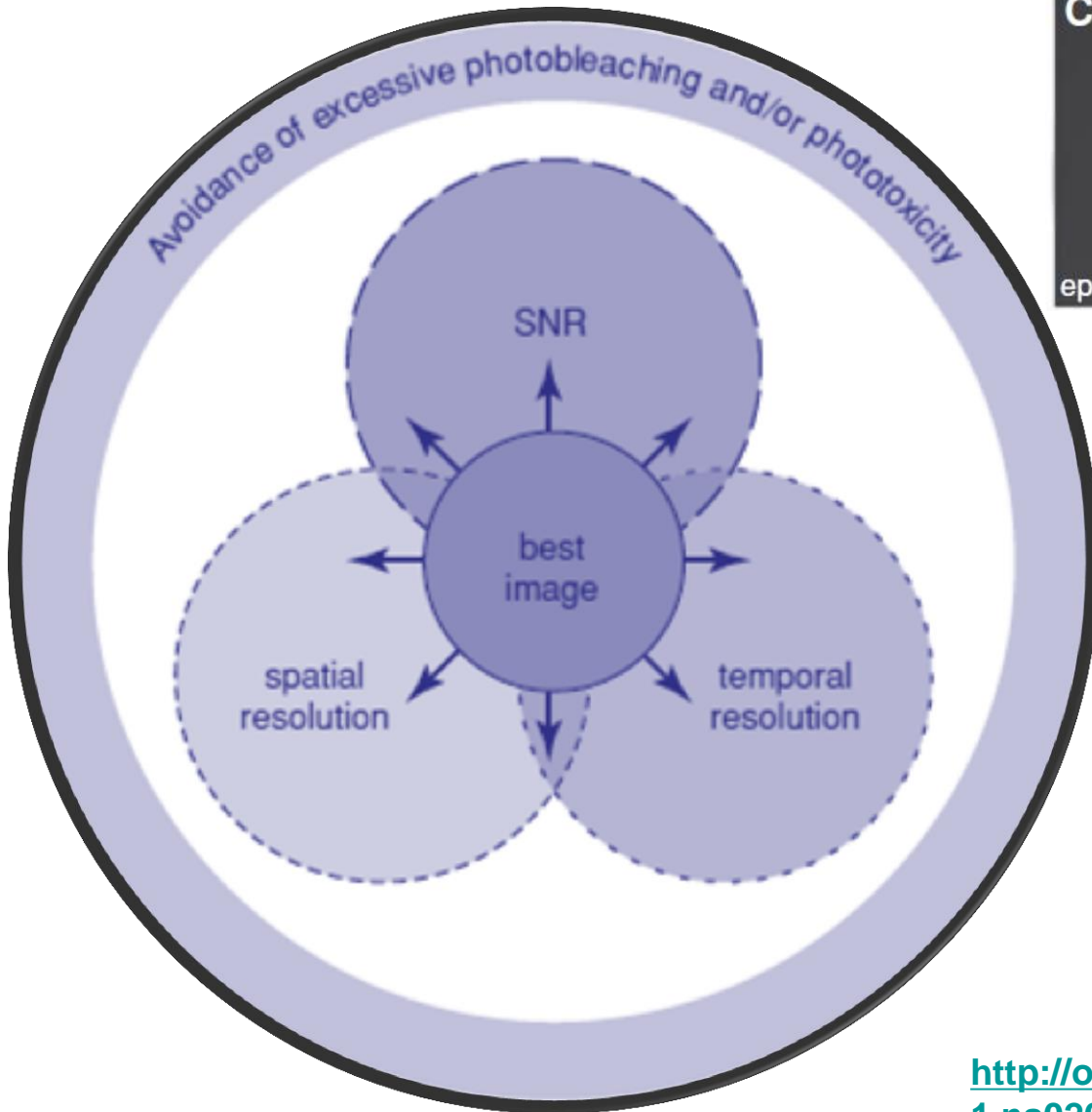




# Part II

## The Resolving Power of a Microscope

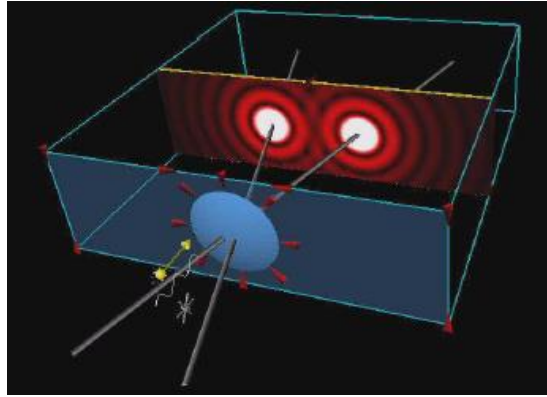
# Diagram of Some of the Critical Opposing Factors in an Imaging Experiment



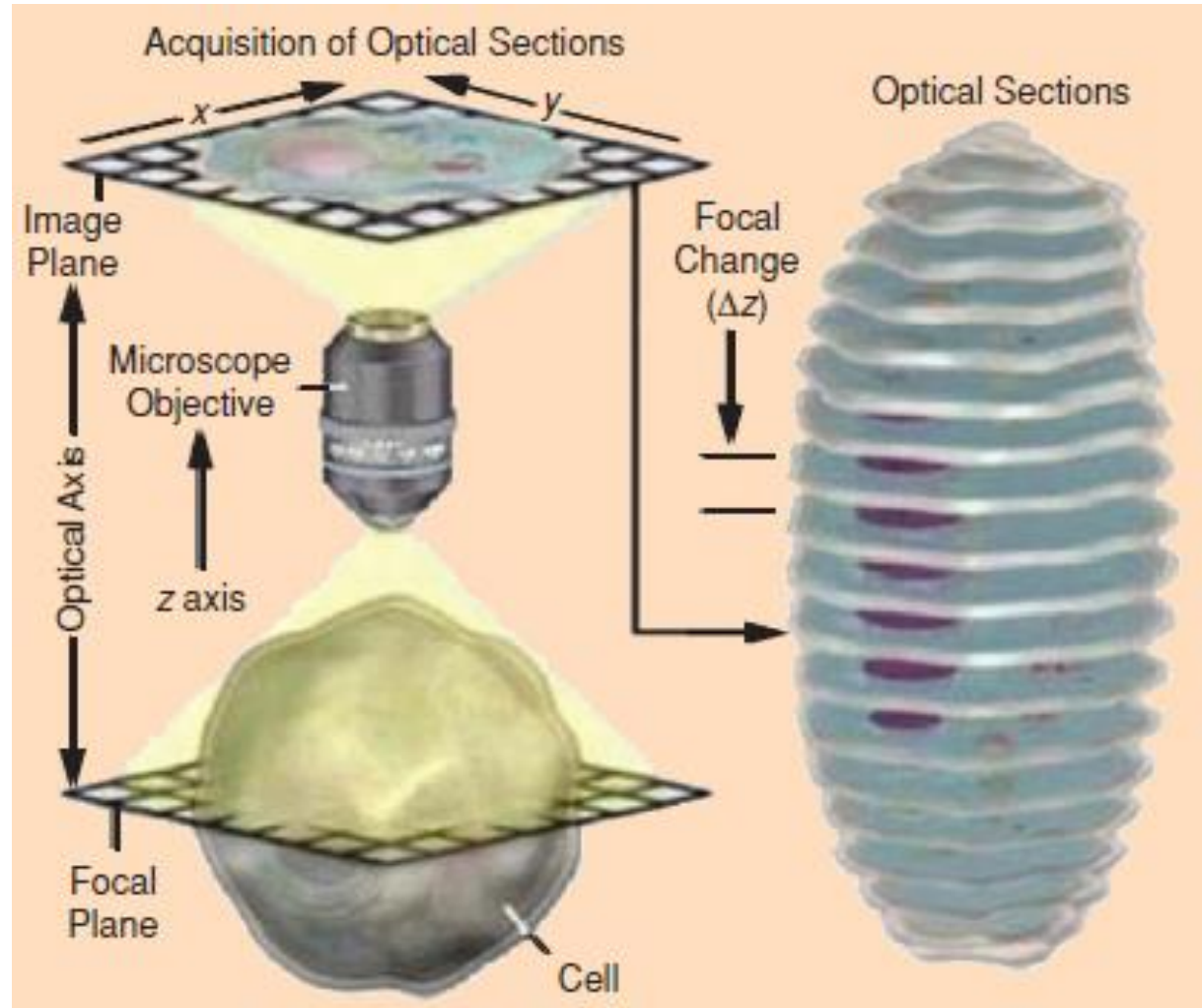
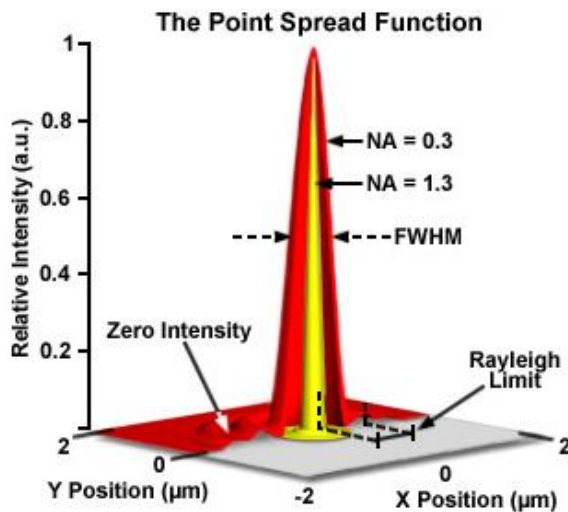


# Physical Limits and Methods to Overcome

An example of the acquired 3-D image of a cell, captured by a fluorescence microscope.



## Point Spread Function (PSF)

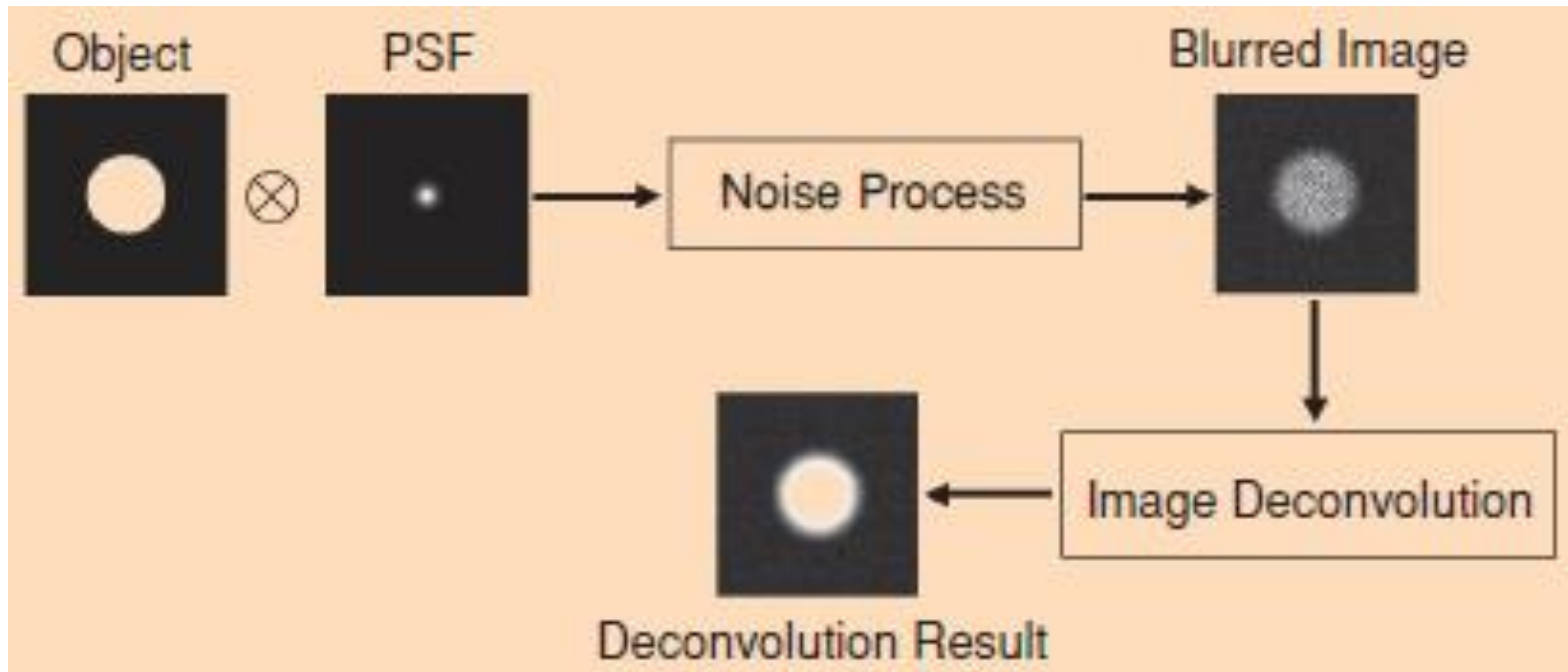
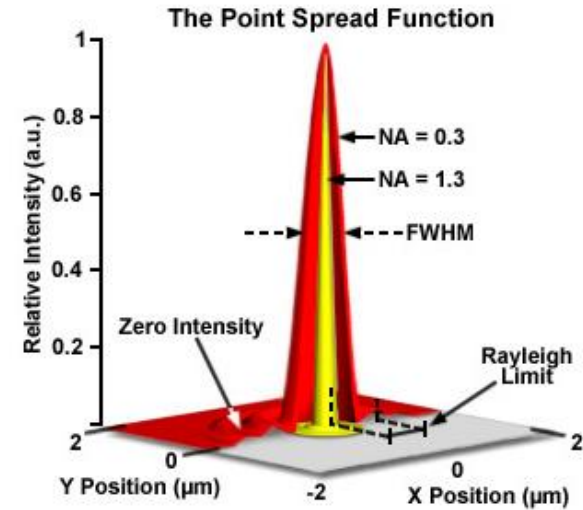
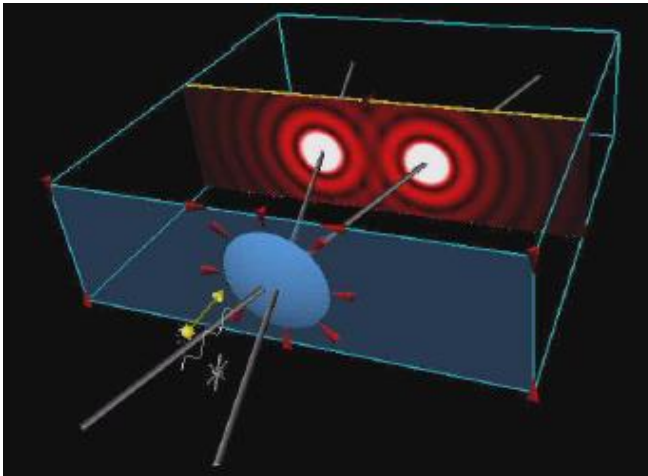


<http://www.es.e.wustl.edu/~nehorai/paper/deconvolutions1.pdf>

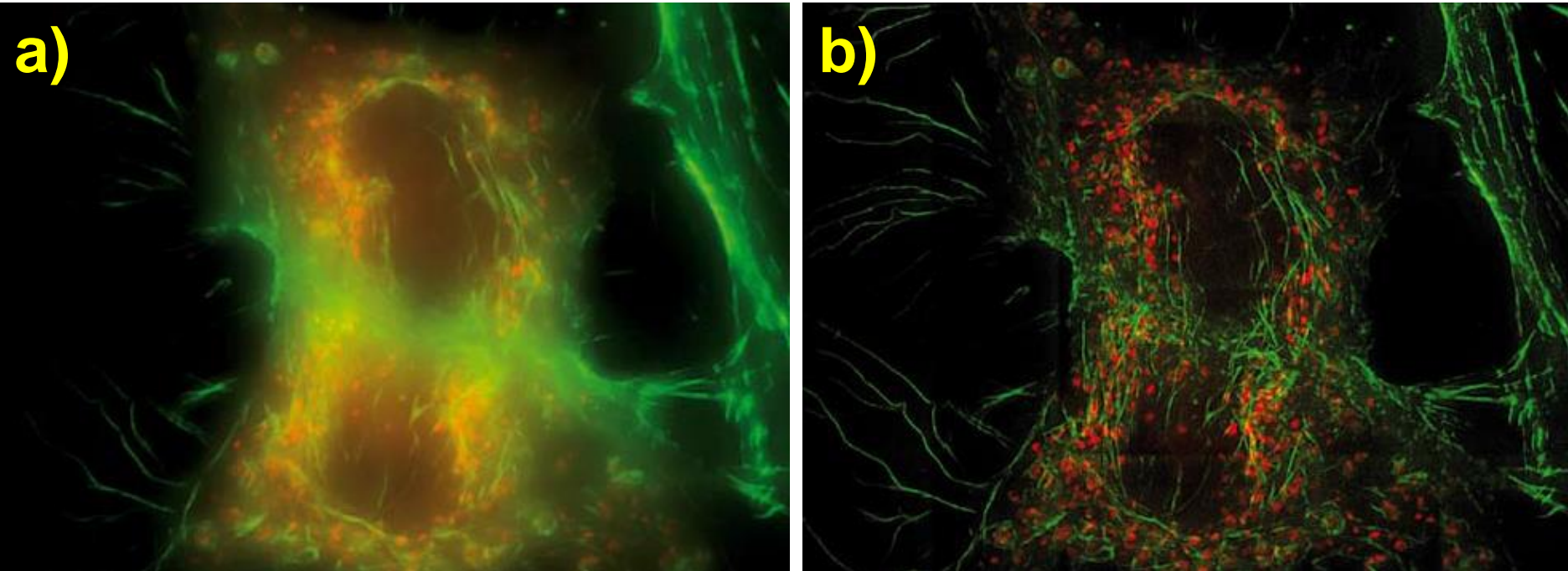
<http://www.olympusmicro.com/primer/digitalimaging/deconvolution/deconintro.html>

<http://zeiss-campus.magnet.fsu.edu/articles/basics/psf.html>

# Physical limits and methods to overcome



# Physical limits and methods to overcome



Via **deconvolution** artefacts can be computed out of fluorescence images.

- a) These artefacts are caused by the stray light from **non-focused areas above and below the focus level**. These phenomena, referred to as convolution, result in **glare** (螢光訊號過亮), **distortion** and **blurriness** (模糊).
- b) Deconvolution is a recognised **mathematical procedure** for eliminating such artefacts. The resulting image displayed is sharper with **less noise** and thus at **higher resolution**. This is also advantageous for more extensive analyses.



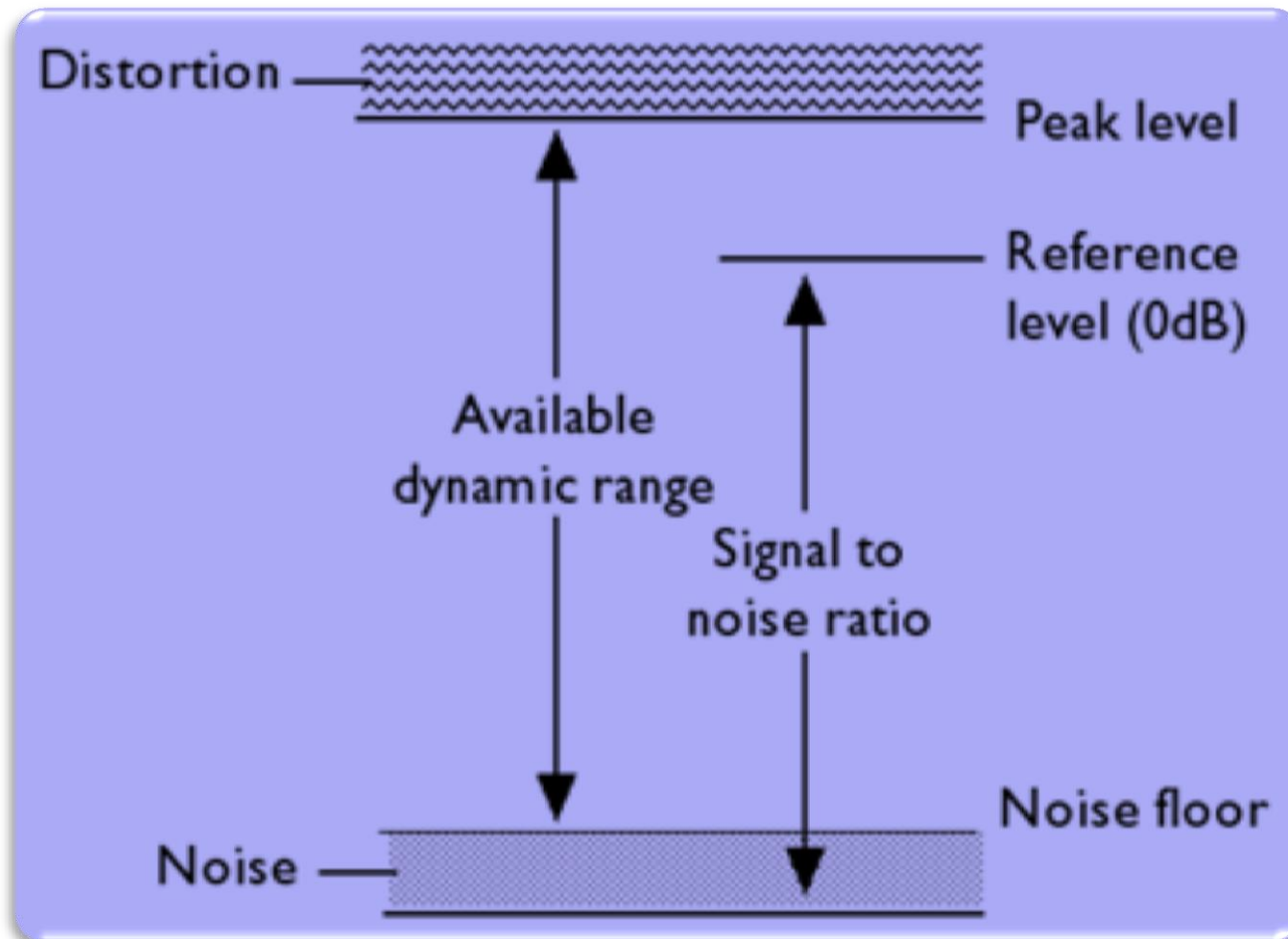
# Part III

## Digital Imaging in Microscope

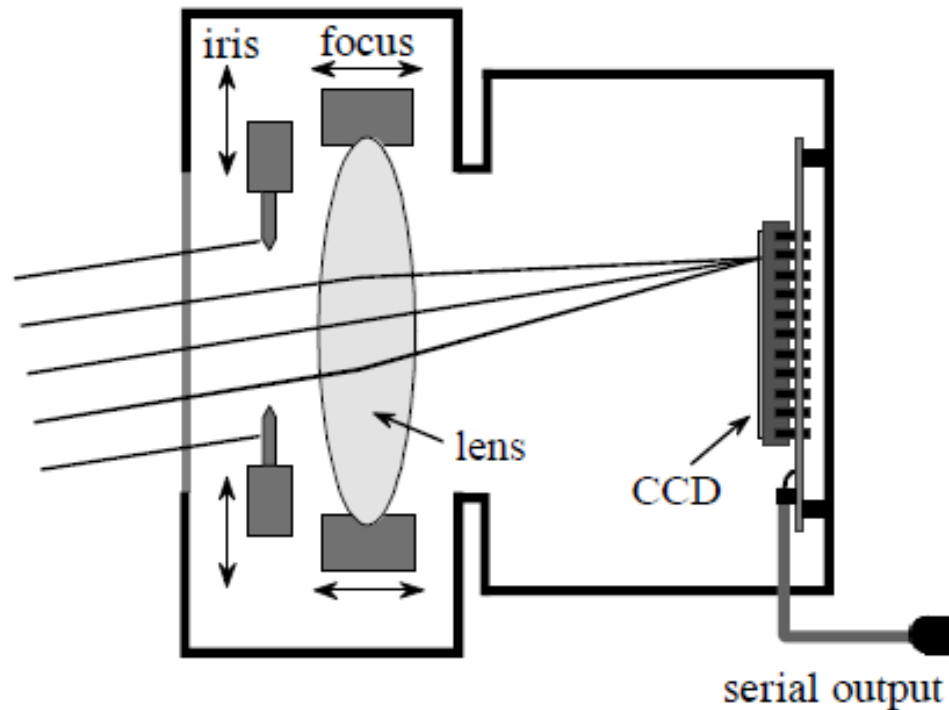


# Dynamic Range vs. SNR

The dynamic range (動態範圍) of a charge-coupled device (CCD): the maximum achievable signal divided by the camera noise.

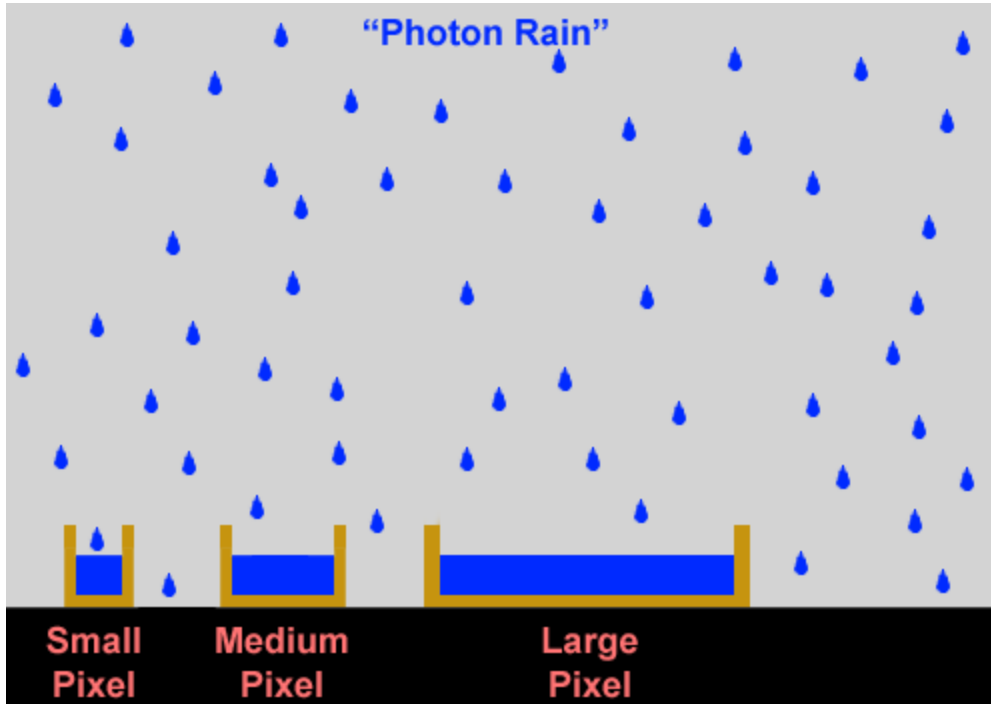


# Diagram of an Electronic Camera



- The most common **imaging sensor** in present day cameras is the **CCD**, a **two-dimensional array of light sensitive elements**.
- Focusing is achieved by moving the lens toward or away from the imaging sensor.
- The amount of light reaching the sensor is controlled by the iris, a mechanical device that changes the effective diameter of the lens.

# Digital Cameras: Does Pixel Size Matter?



泊松分佈 (Poisson distribution)

$$\therefore \text{SNR} = n / n^{1/2} = n^{1/2}$$

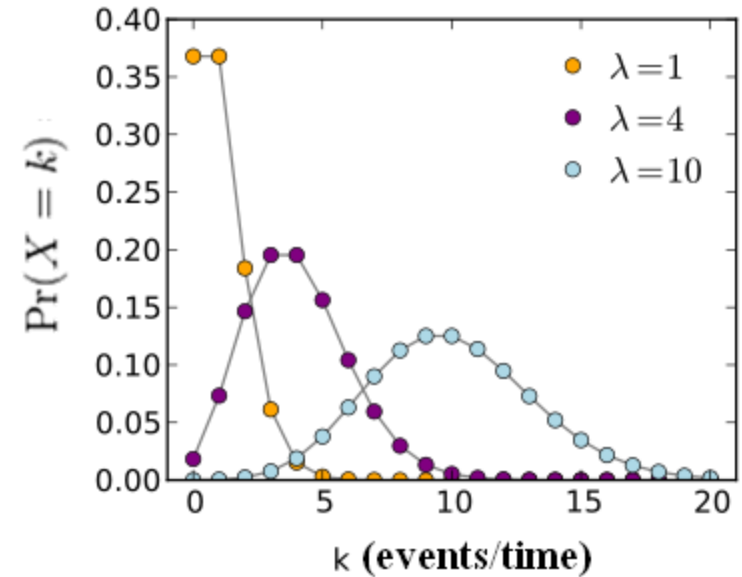
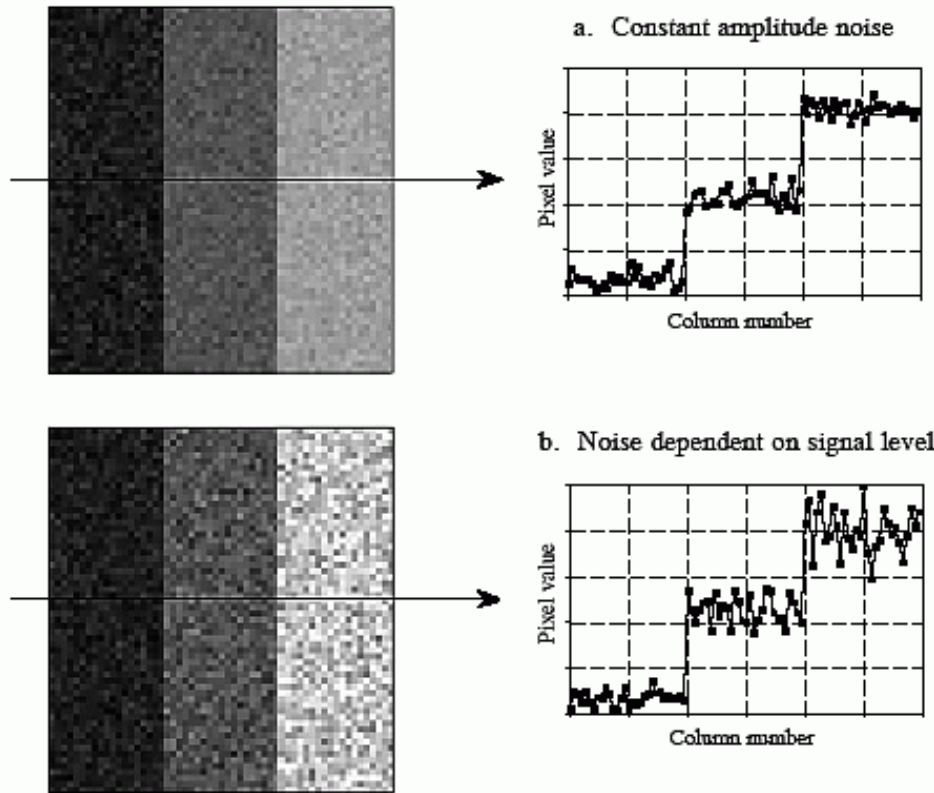
Photons	Noise	signal-to-noise
9	3	3
100	10	10
900	30	30
10000	100	100
40000	200	200

➤ In the physics of **photon counting**, the **noise** in the signal is equal to the **square root of the number of photons**.

- The larger the bucket, the more drops that can be collected in a given amount of time.
- The accuracy of the signal measured is directly proportional to the size of the signal.

# Image Noise: **shot noise** (electronic noise)

泊松分佈 (Poisson distribution)



$$\Pr(X = k) = \frac{\lambda^k e^{-\lambda}}{k!},$$

$\lambda$ : 平均發生率 (mean rate)

→ mean events/time

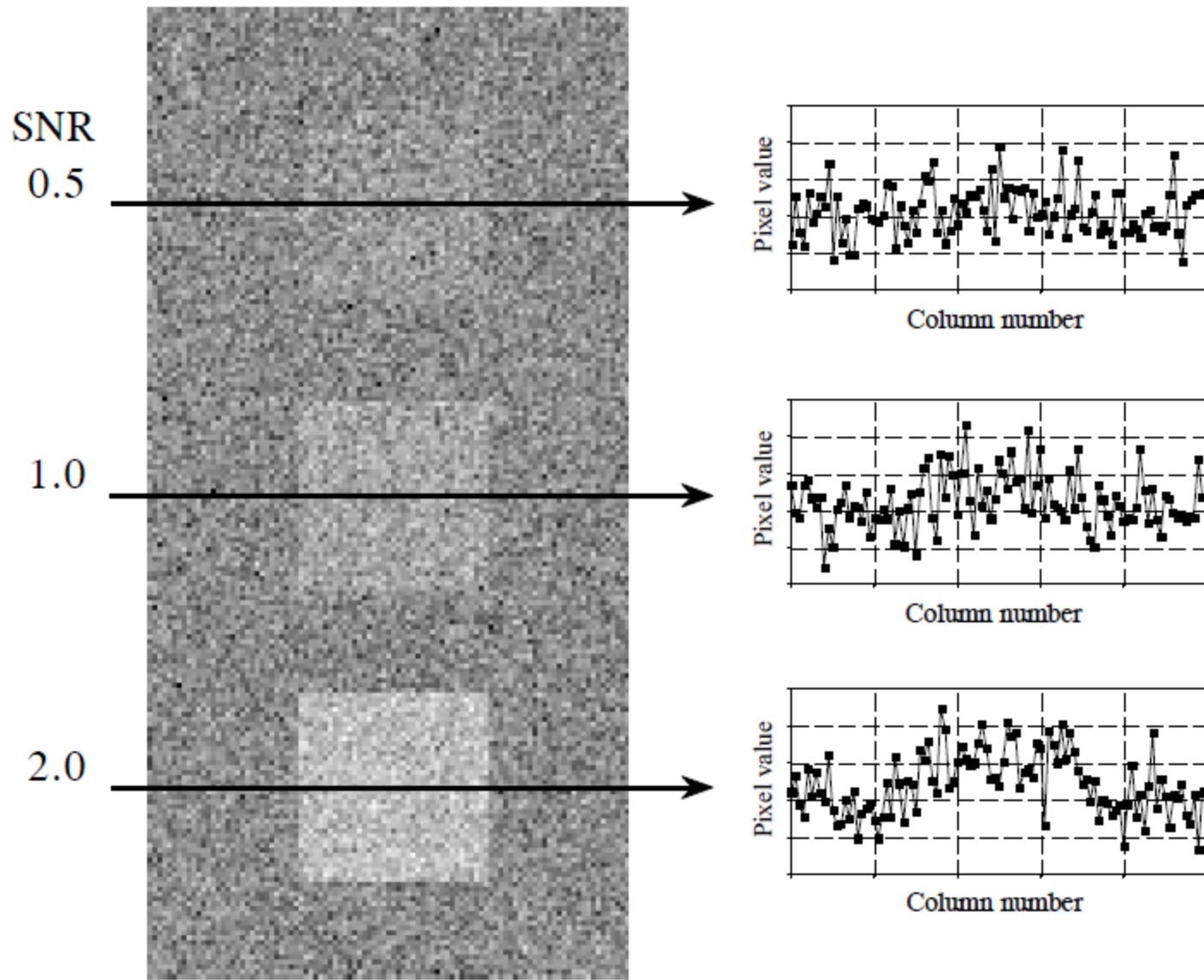
Random noise in images takes two general forms.

➤ In (a), the amplitude of the noise remains constant as the signal level changes. This is typical of electronic noise.

➤ In (b), the amplitude of the noise increases as the square-root of the signal level. This type of noise originates from the detection of a small number of particles, such as light photons, electrons, or x-rays.



# Signal-to-noise ratio (SNR)

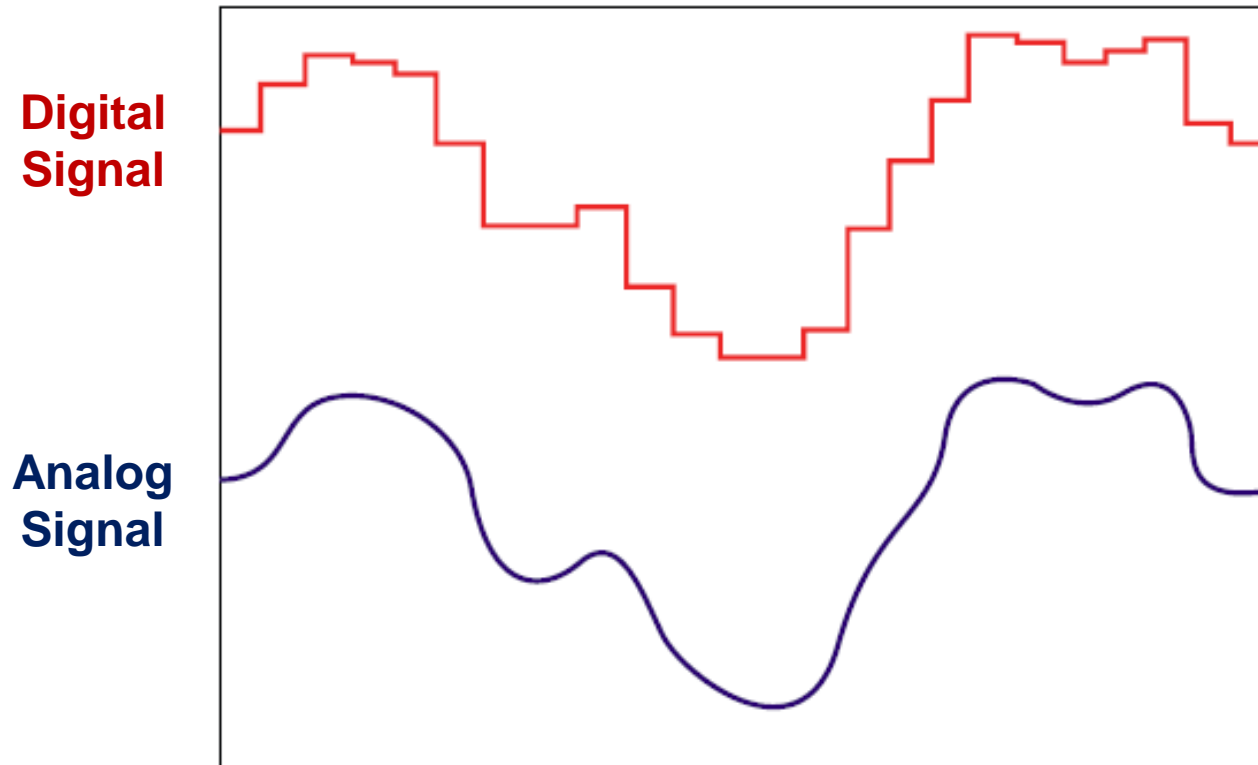


➤ An object is visible in an image only if its contrast is large enough to overcome the random image noise. 25

# Basic Imaging Concepts

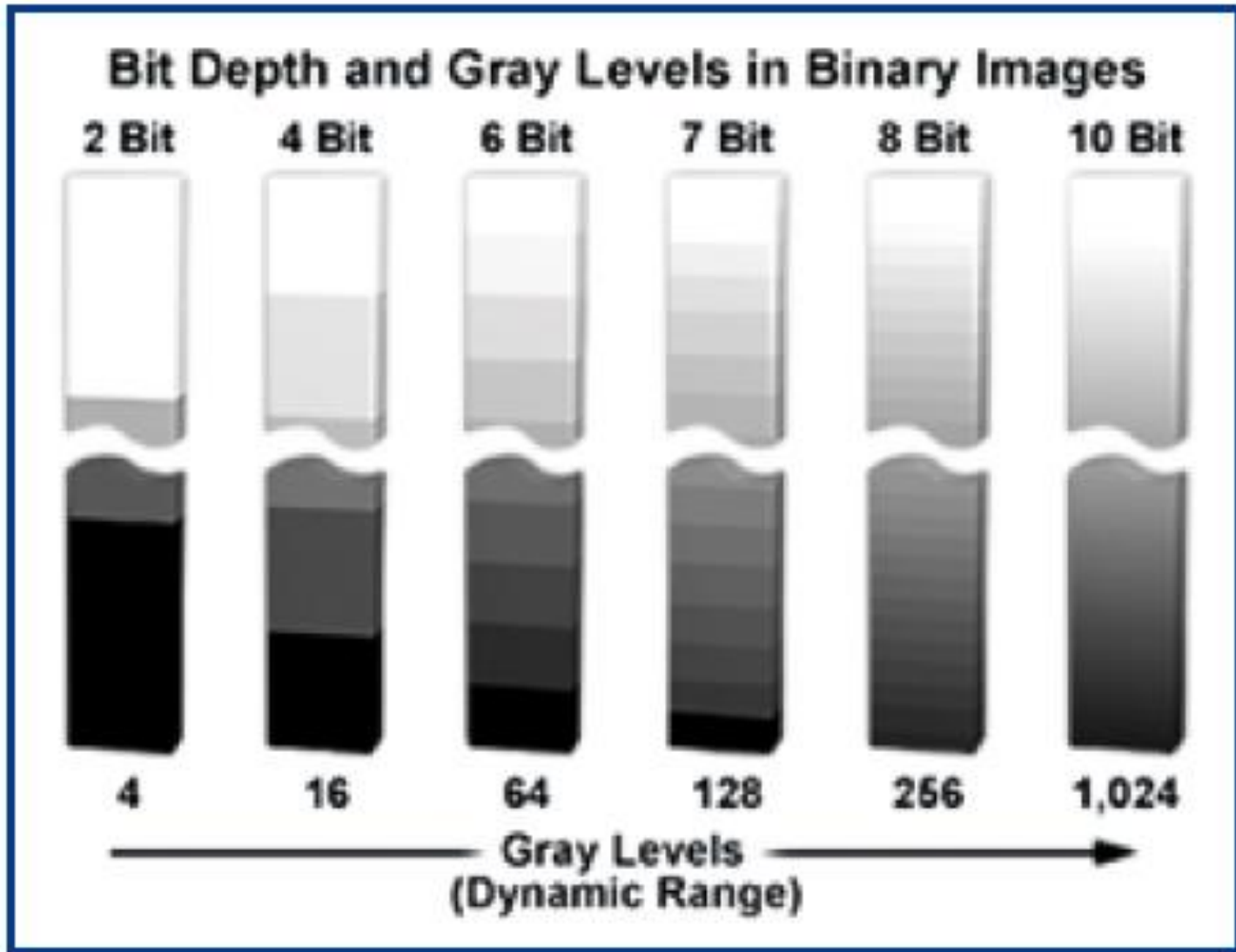
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## Digital Image Acquisition: Analog to Digital Conversion

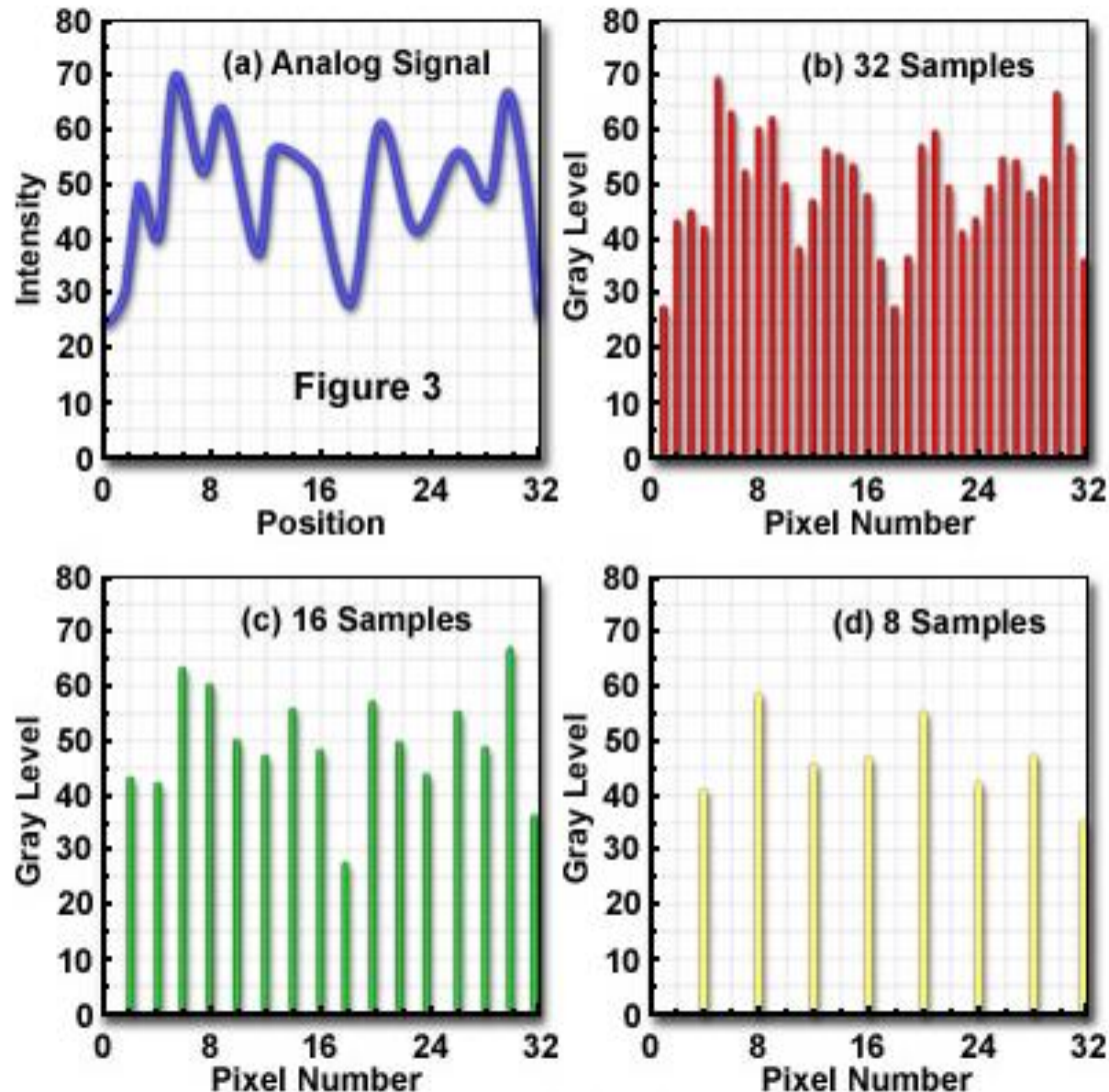


**Digitization** of an analog voltage signal along one line in an image (blue) produces a series of values that correspond to a series of steps (red) equal in time and rounded to integral multiples of the smallest measurable increment.

# Bit depth and grey levels in digital images



# Bit depth and grey levels in digital images

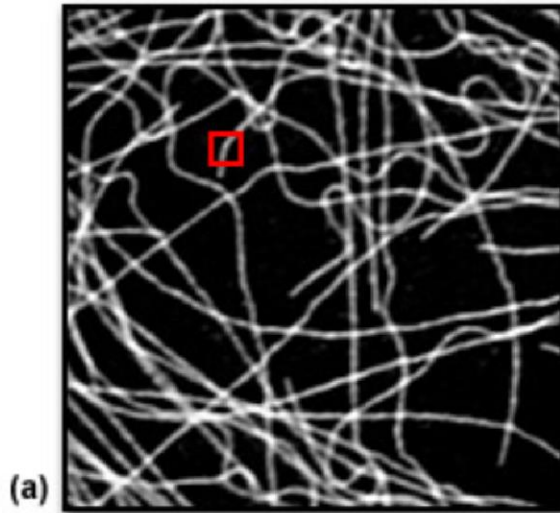




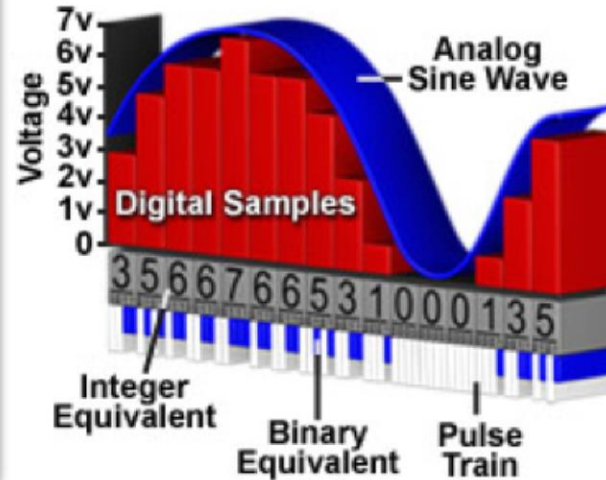
# Basic Imaging Concepts

## Digital Image Acquisition: Analog to Digital Conversion

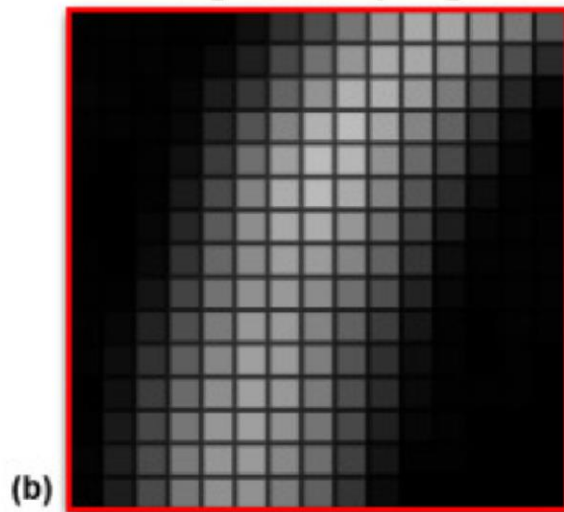
Analog Imaging



Analog and Digital Signals



Digital Sampling



Pixel Quantization

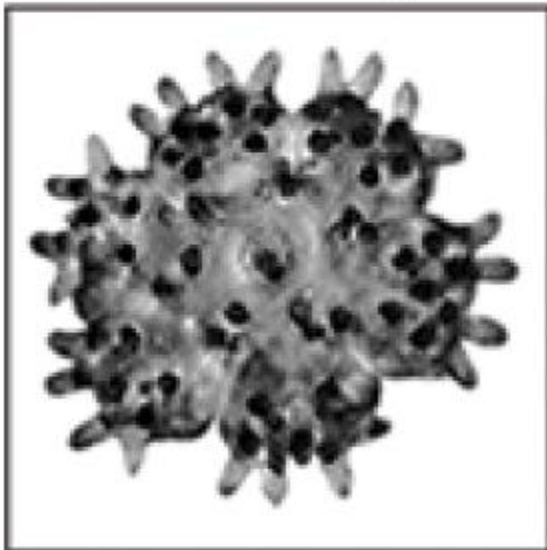
(c)

2	3	3	2	3	16	47	78	118	152	170	165	149	119	83
3	2	3	3	11	31	72	113	150	170	168	148	118	78	41
5	3	2	7	28	51	100	147	177	175	155	123	82	38	10
3	3	3	8	41	83	132	177	188	165	132	98	52	15	0
2	0	3	16	59	111	160	188	181	145	105	72	31	7	0
0	0	3	26	75	131	172	186	170	132	85	47	13	3	2
0	0	7	38	90	141	168	172	150	113	67	28	5	3	2
2	0	10	51	103	139	159	155	132	98	52	13	3	3	3
2	2	20	67	114	144	152	139	111	78	34	8	2	3	3
3	7	34	78	123	152	154	131	96	60	21	3	0	3	2
3	13	49	93	134	159	154	126	83	47	13	3	0	2	0
0	16	60	106	142	160	152	123	78	43	10	2	2	2	0
2	25	70	118	150	159	145	116	72	31	7	3	0	0	0
5	31	74	123	149	154	136	110	64	21	2	2	0	0	0
3	29	74	119	144	145	124	96	52	11	0	0	0	0	0

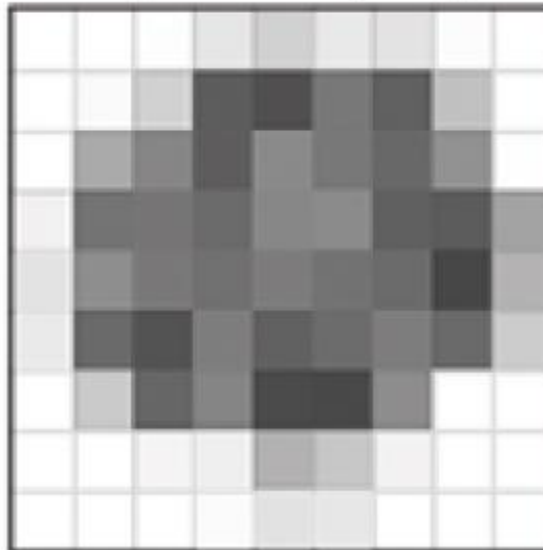
# Creation of a Digital Image

## Creation of a Digital Image

Analog Image



Digital Sampling



Pixel Quantization

249	244	240	230	209	233	227	251	255
248	245	210	93	81	120	97	193	254
250	170	133	94	137	120	104	145	253
241	116	118	107	134	138	96	92	163
277	142	121	113	124	115	107	71	179
234	106	84	125	97	100	125	106	204
241	202	102	132	75	73	141	246	252
253	252	244	239	178	199	242	250	245
255	249	244	250	226	231	240	251	253

# Resolution in Digital Images – is it important?

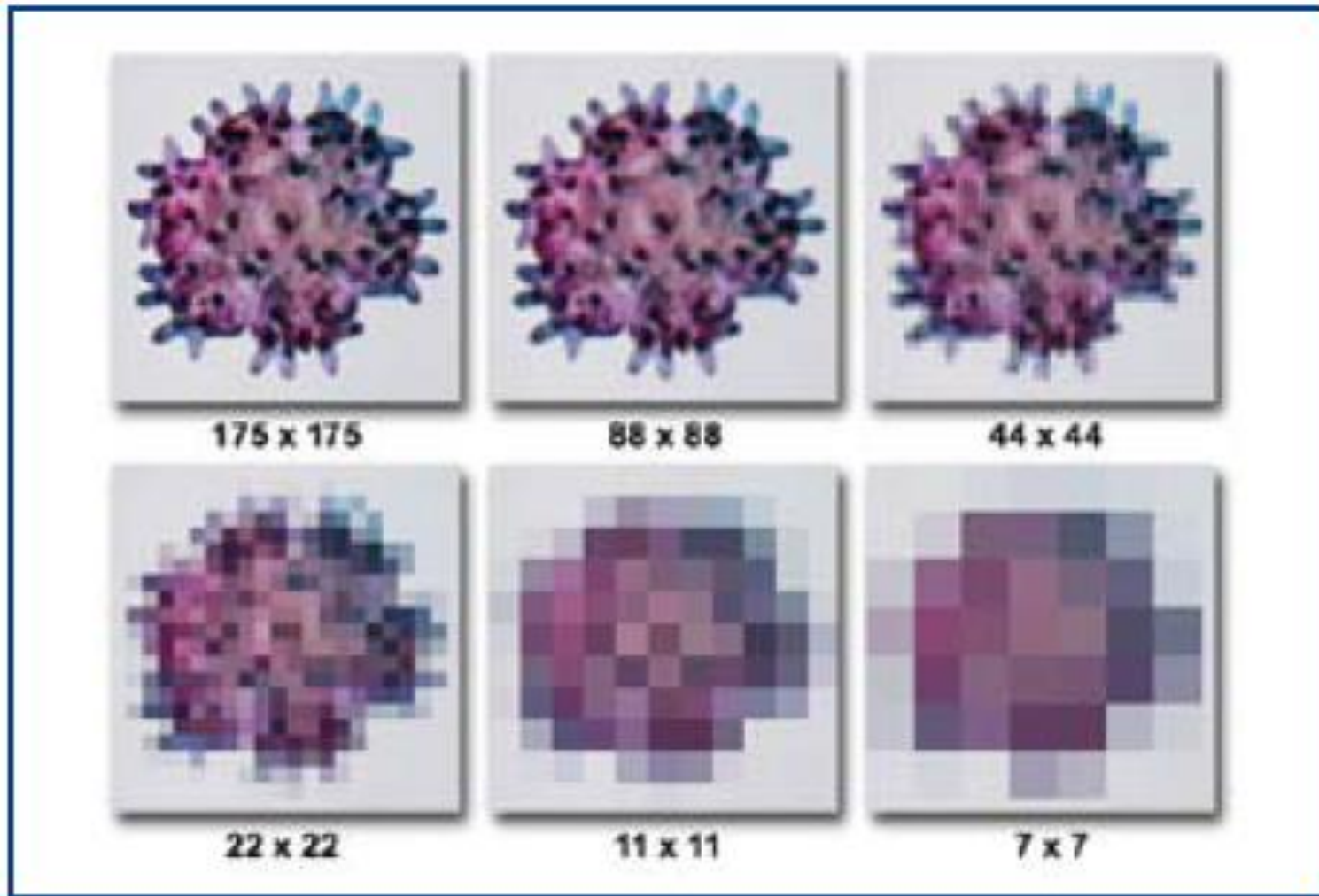


Fig. 17: Four representations of the same image, with different numbers of pixels used. The numbers of pixels is written below each image.

$256 \times 256$



$128 \times 128$



$64 \times 64$



$32 \times 32$



Four representations of the same image, showing a variation in the number of pixels used. In all cases, **a full 256 gray values are retained**. Each step in coarsening of the image is accomplished by **averaging the brightness of the region covered by the larger pixels**.



32



16



8



4



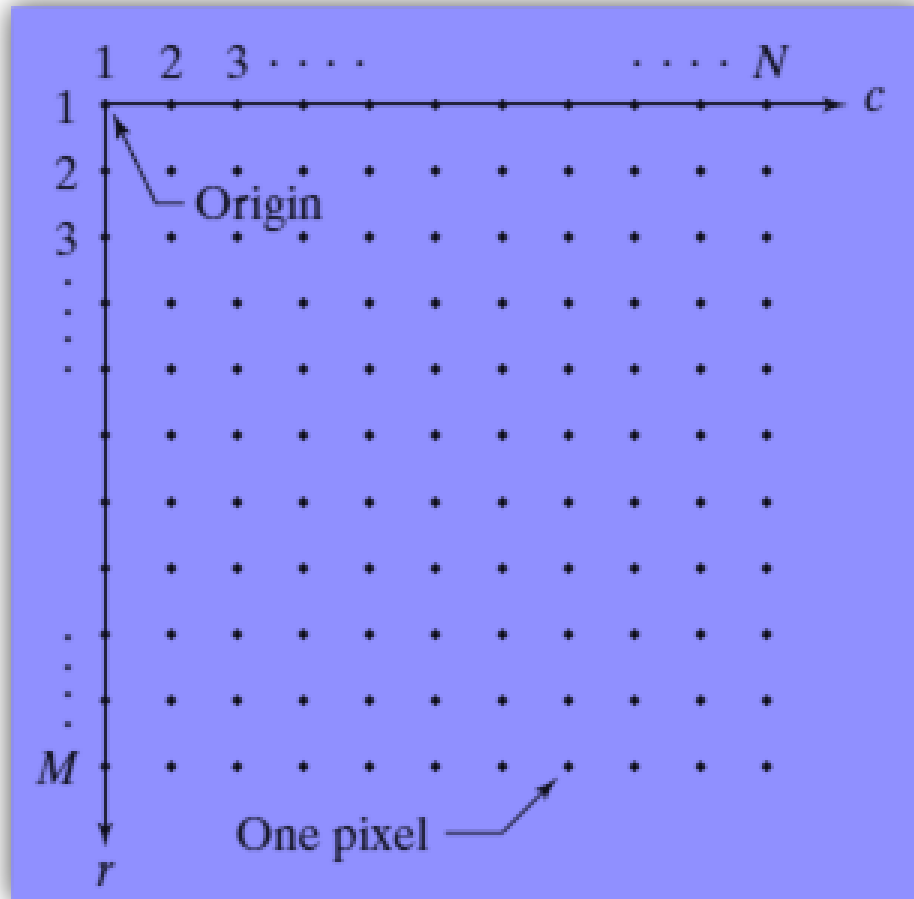
Four representations of the same image, with **variation in the number of gray levels used**. From the upper left: 32; 16; 8; 4. In all cases, a full  $256 \times 256$  array of pixels is retained. Each step in the coarsening of the image is accomplished by rounding the brightness of the original pixel value.

# Part IV

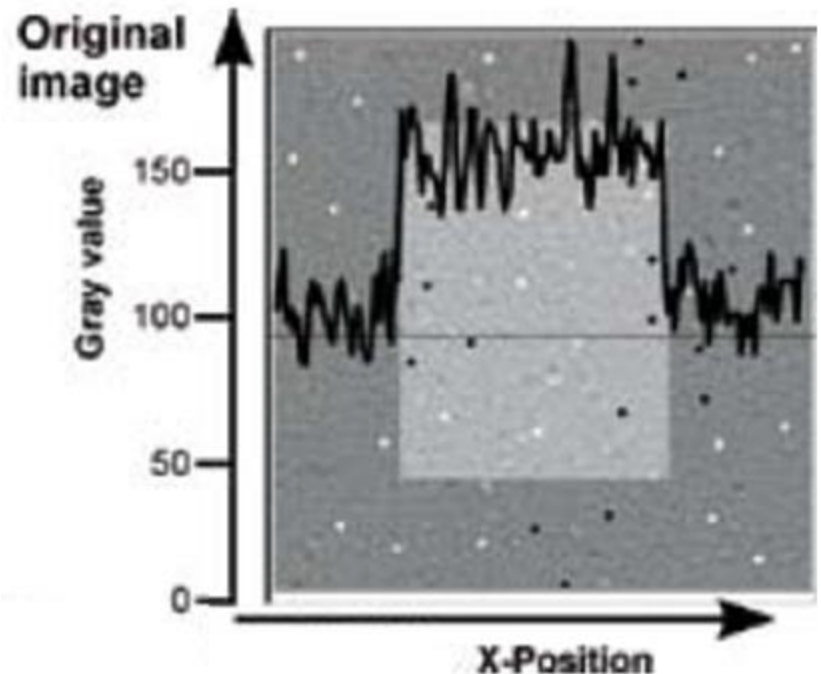
## The Fundamentals of Imaging Processing

# Coordinate Convention in the Image Processing

## Array Indexing



```
>> f = imread('chestxray.jpg');  
>> f = imread('D:\myimages\chestxray.jpg');  
>> imshow(f);  
>> imwrite(f, 'DT.bmp')
```



# Coordinate Convention in the Image Processing

---

## Example

```
A =
```

1	2	3
4	5	6
7	8	9

```
>> T2 = A(1:2, 1:3)
```

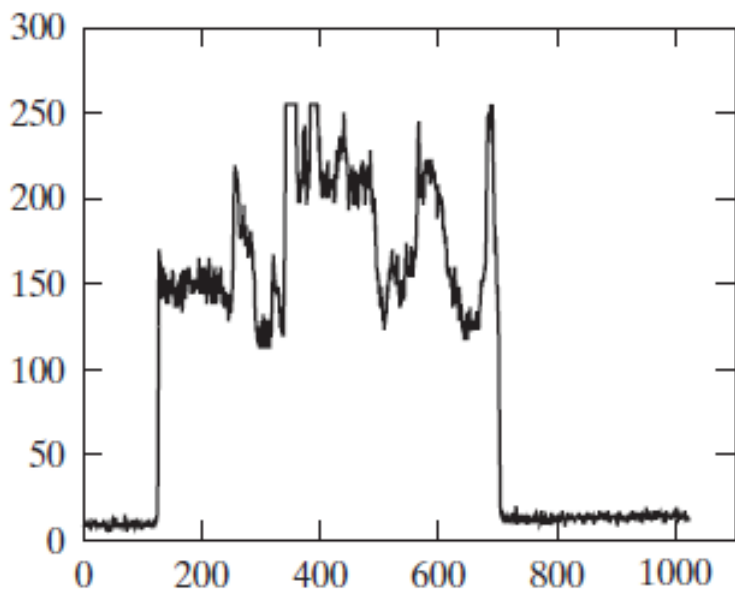
```
T2 =
```

1	2	3
4	5	6



# Coordinate Convention in the Image Processing

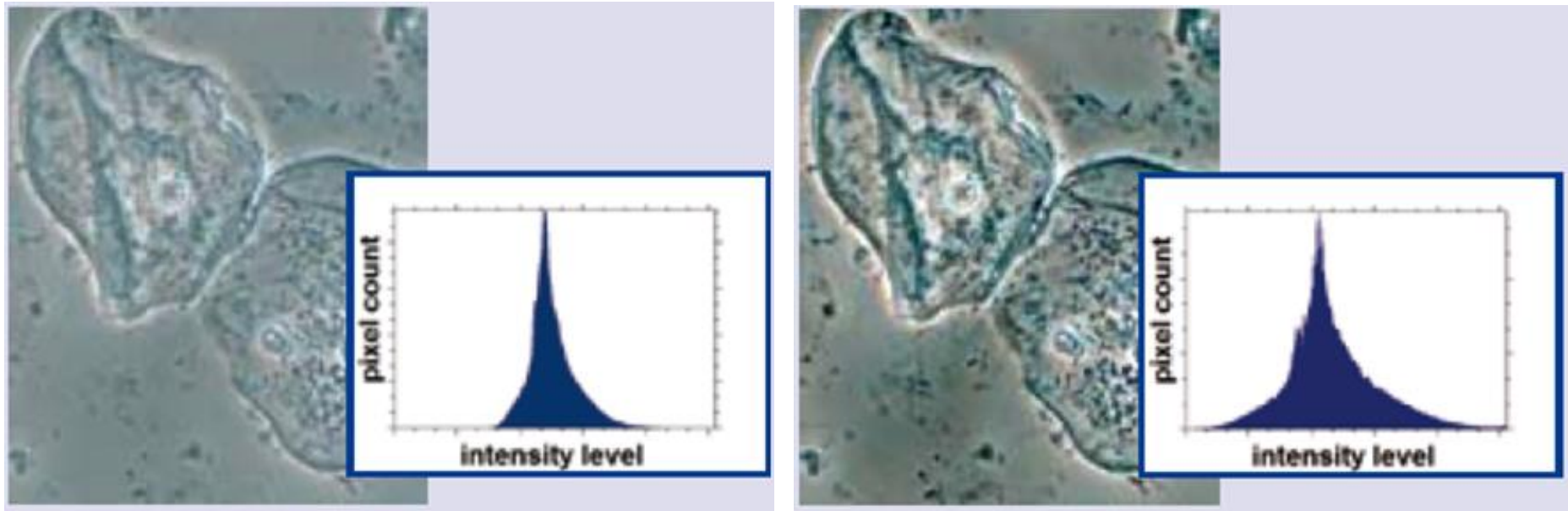




a b c  
d  
e

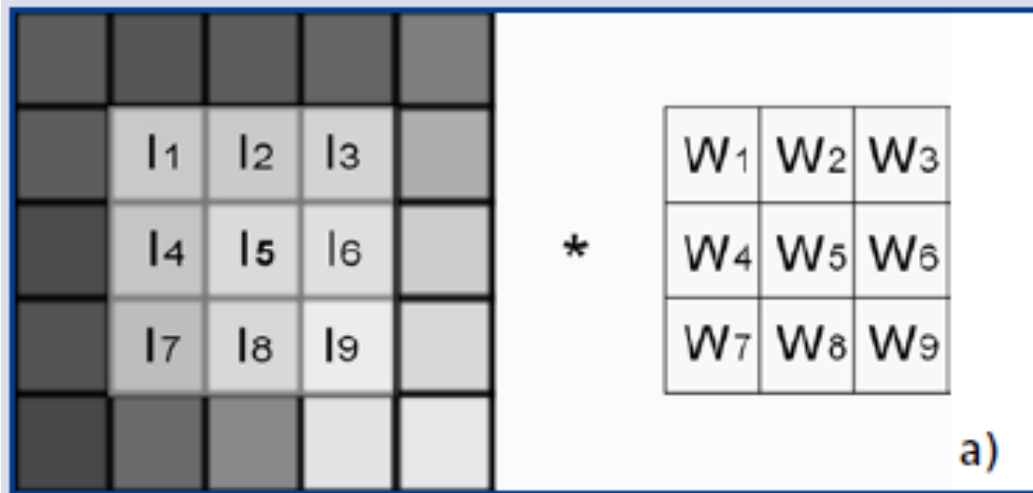
Results obtained using array indexing.  
(a) Original image. (b) Image flipped vertically (垂直翻轉). (c) Cropped image (裁剪). (d) Subsampled image. (e) A horizontal scan line through the middle of the image in (a).

# Histogram Optimisation During Acquisition



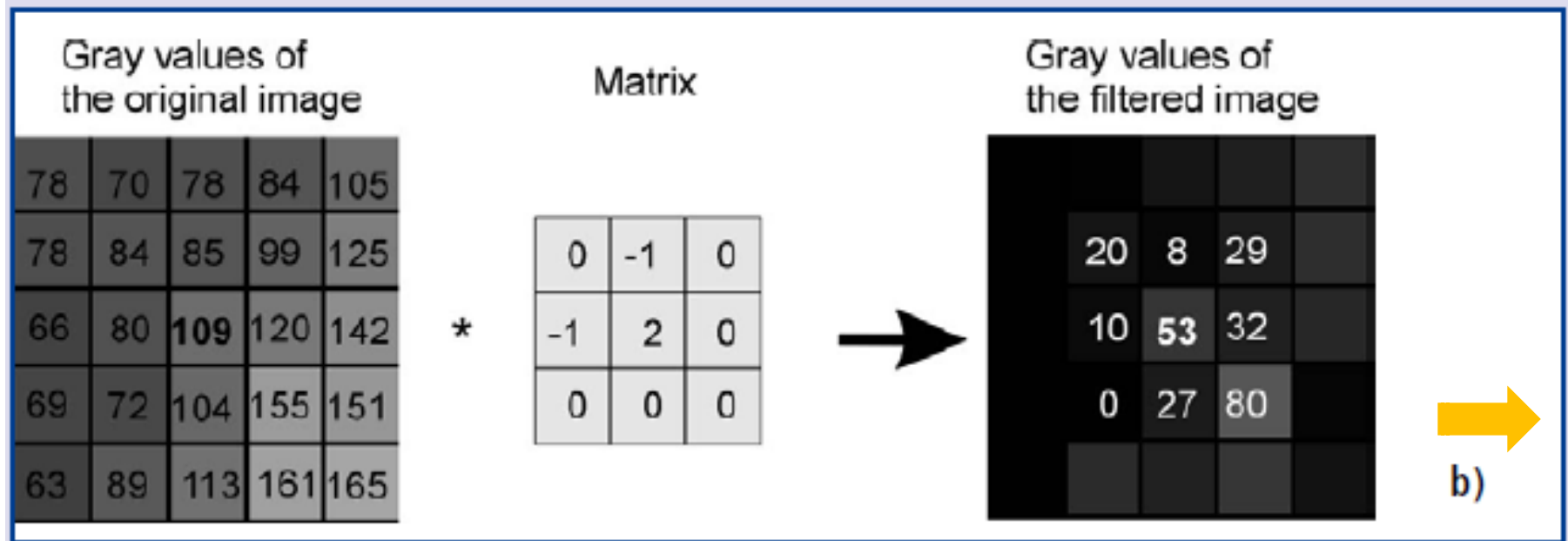
Left side with low contrast setting, right side with contrast optimisation of microscope system and camera setting.

# How to describe **image processing operations** mathematically



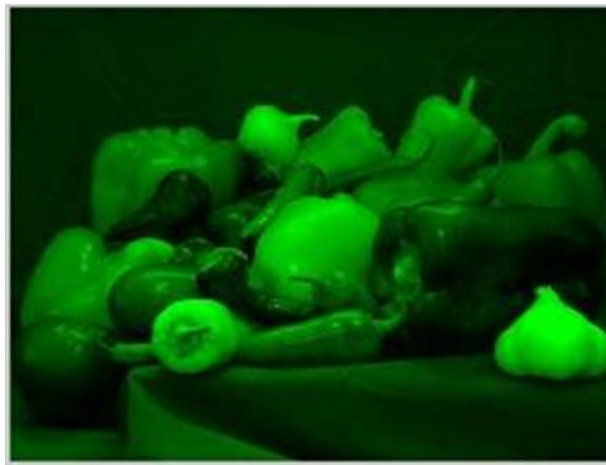
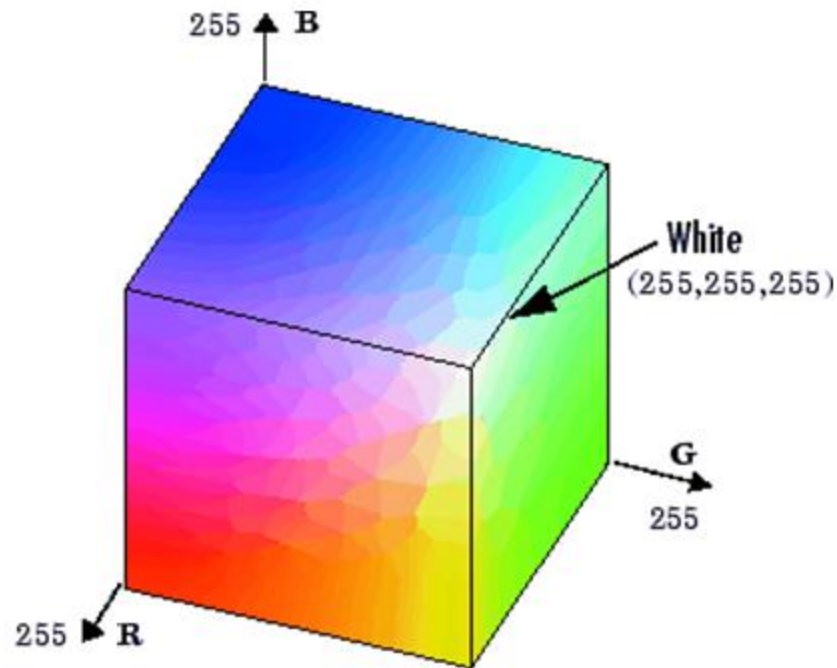
## Local Operations:

Many well known **noise reduction**, **sharpening** and **edge enhancing filters** are convolution filters.





# RGB Image Decomposition



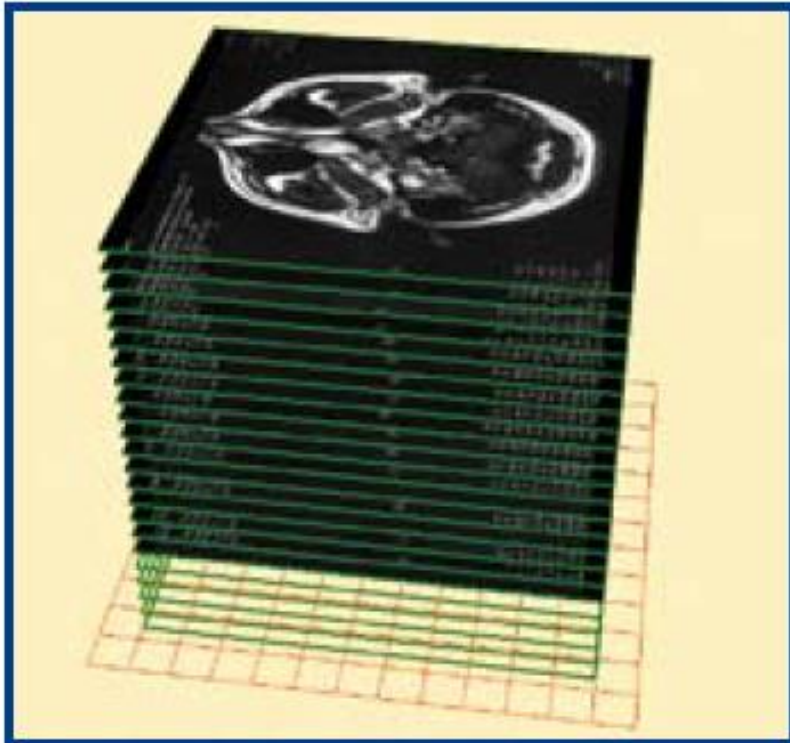
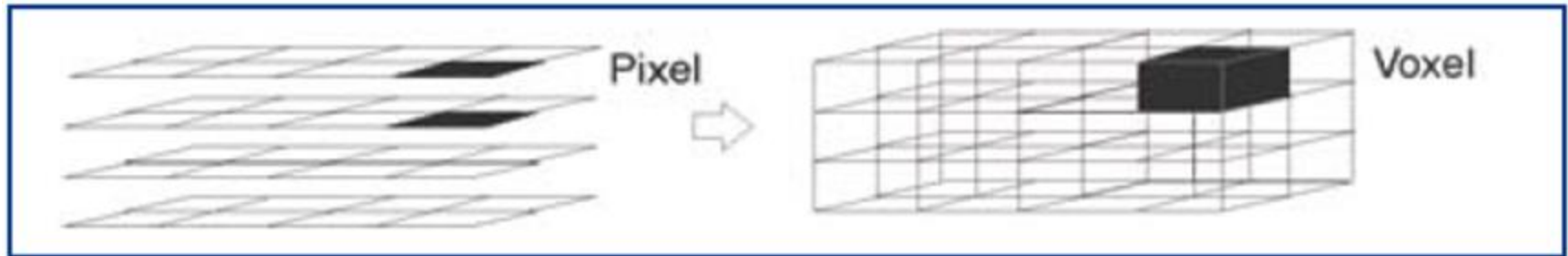
# Visual Shade Matching



The appearance of a tooth is the summation of light that is reflected, transmitted, and fluoresced.



# 3-D Reconstruction using an image series of specimen sections



This is how a two-dimensional **pixel** (像素/picture element) is expanded to a three-dimensional **voxel** (體素/volume element).



# Thanks For Your Attention

